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Pixel array for 3-D integration with an intra-cortical electrode array.

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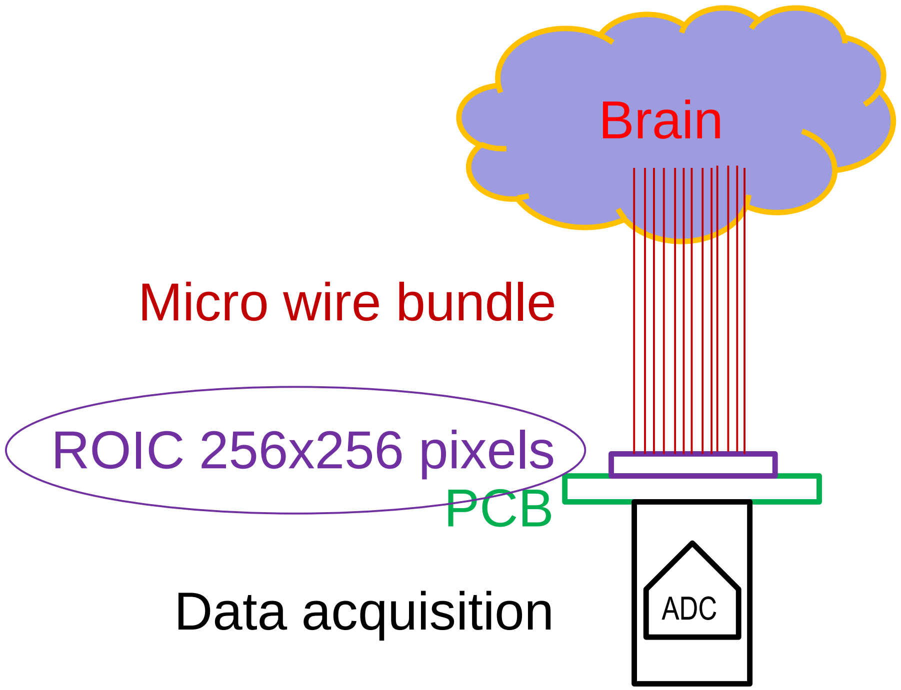
Outline

1. Introduction, purpose
   - ⇒Direct extracellular neuron signal sensing
   - ⇒Our approach
2. Pixel design & performance
   - ⇒Sense amplifier design
   - ⇒Measured performance
3. Future outlook
   - ⇒In-pixel analog domain filtering
   - ⇒Prototype results



1. Introduction: purpose

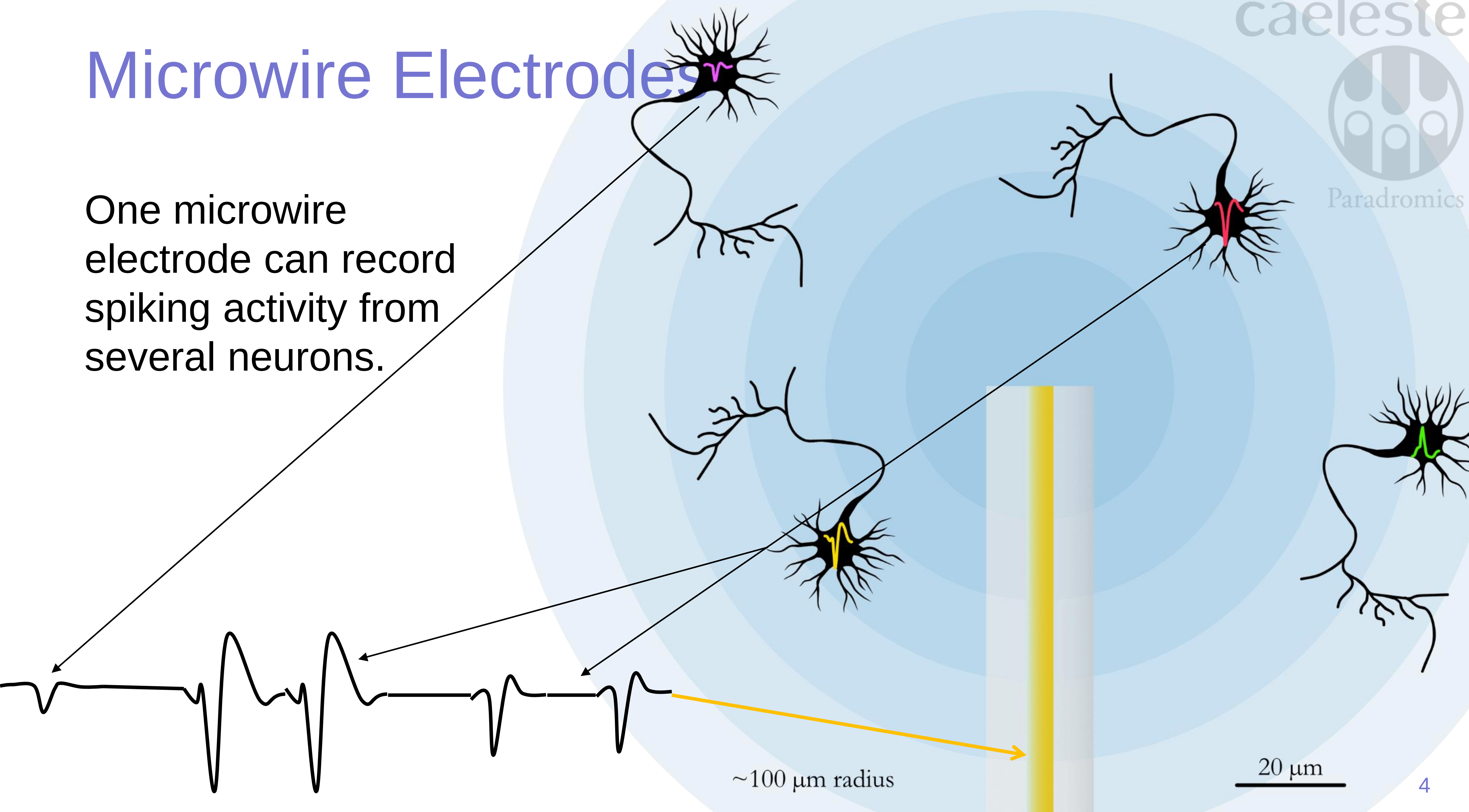
Detecting neural events in the brain

→ by an array of microelectrodes connected to an array of voltage amplifiers

→ like a large channel count oscilloscope with 10µV 20kHz resolution

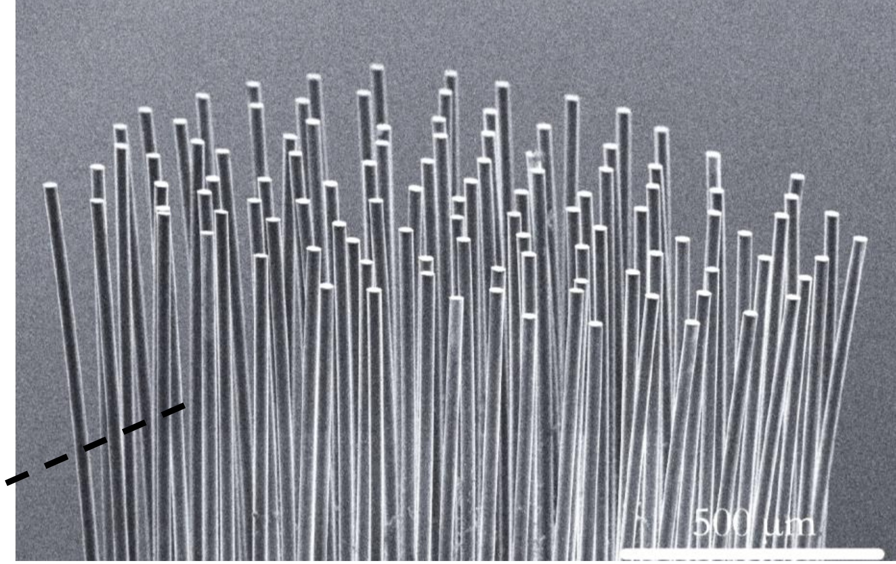
Microwire Electrodes

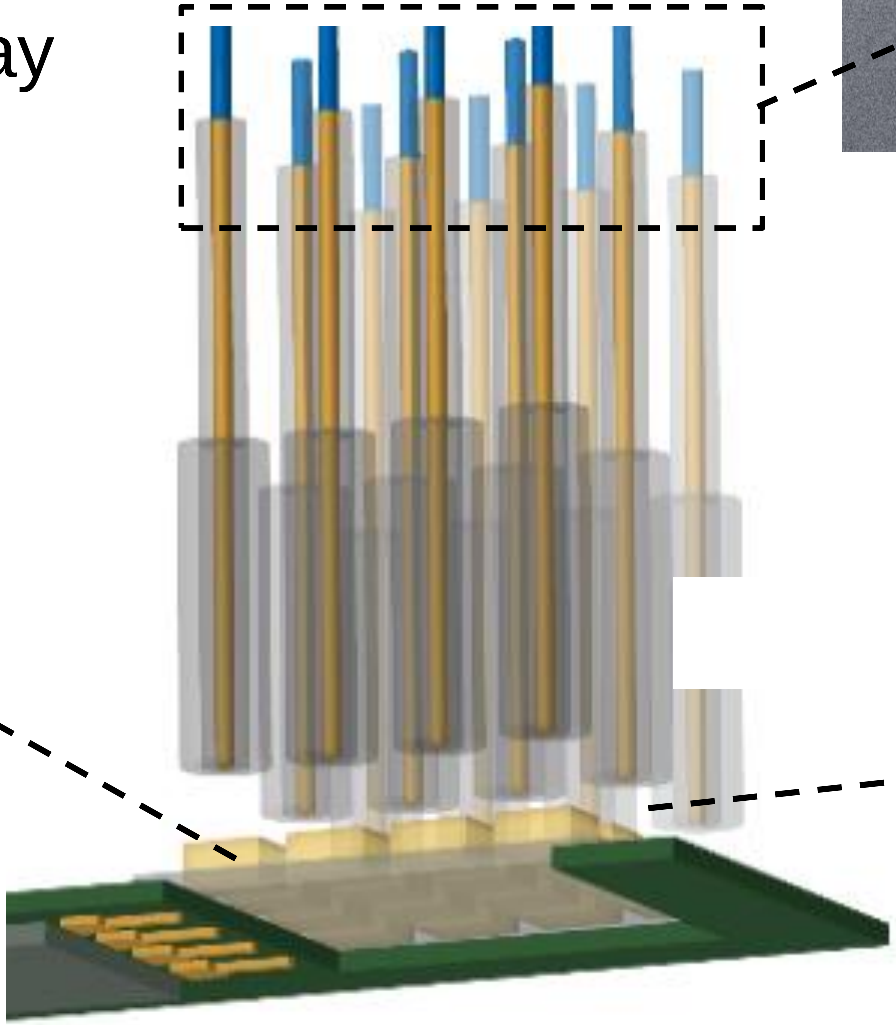
One microwire electrode can record spiking activity from several neurons.

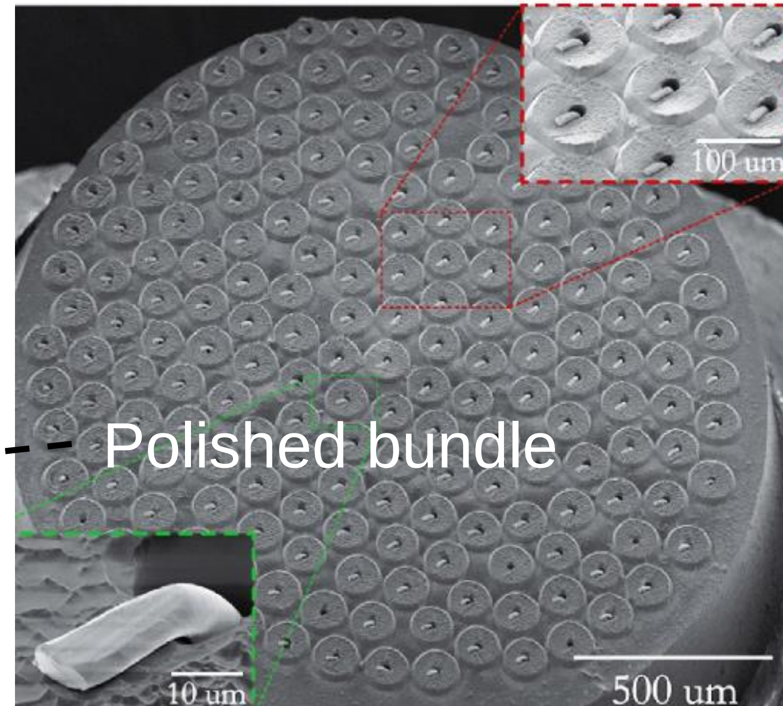


Recording from microwire electrodes

Connecting microwires directly to a CMOS array allows for readout, digitization, and multiplexing.

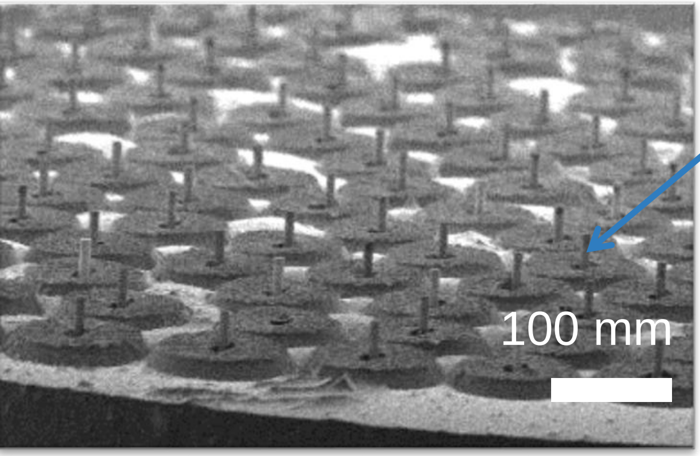




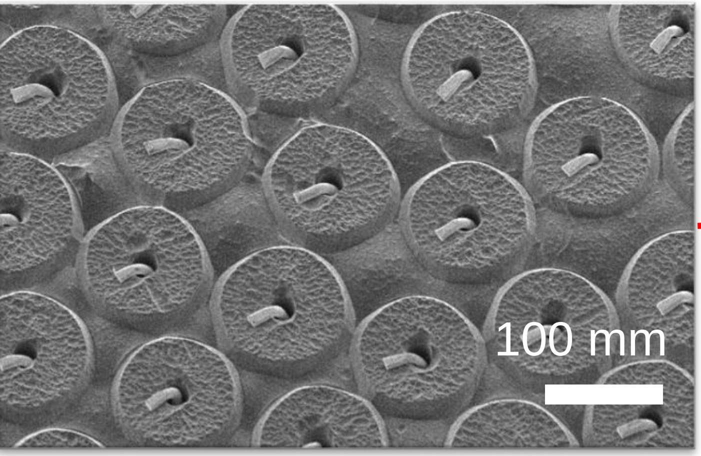


Press the bundles onto CMOS sensor

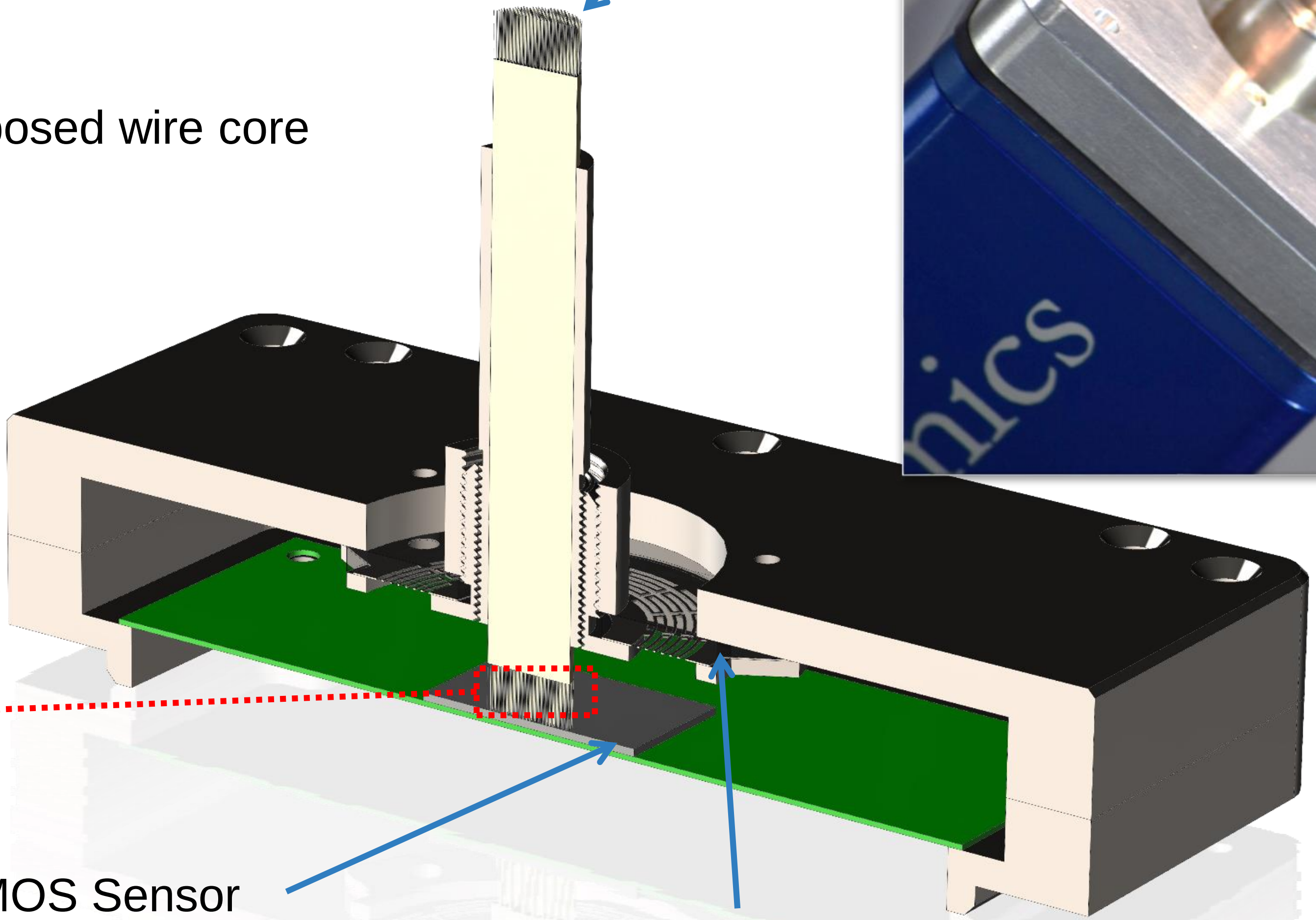
Bundle before Pressing



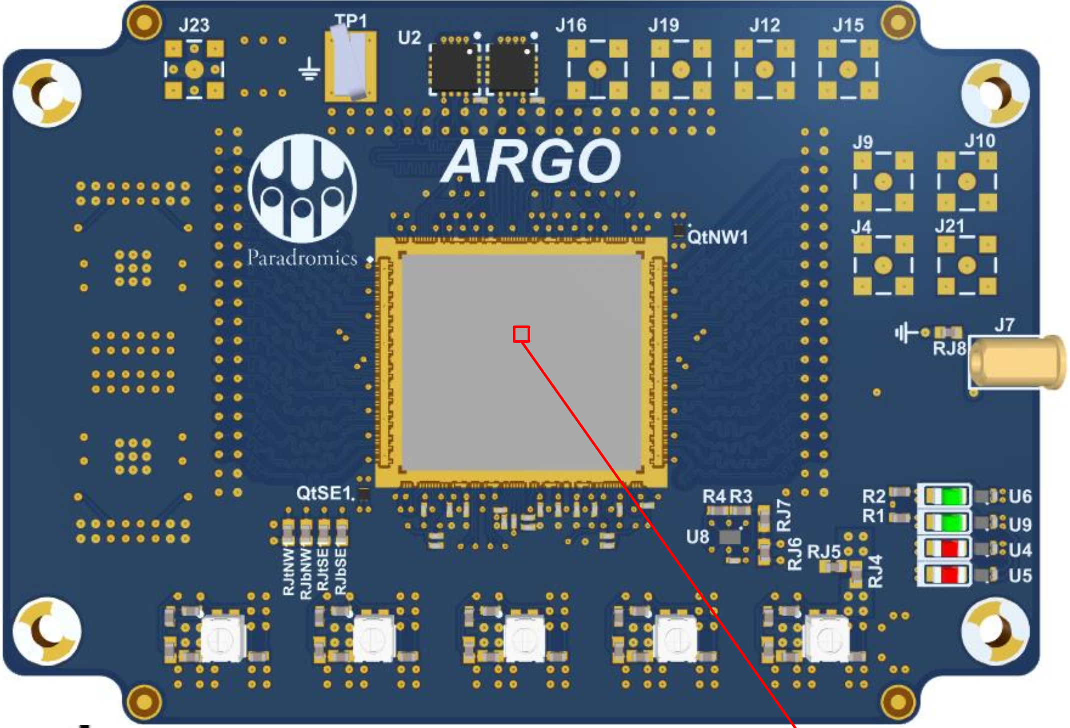
Exposed wire core

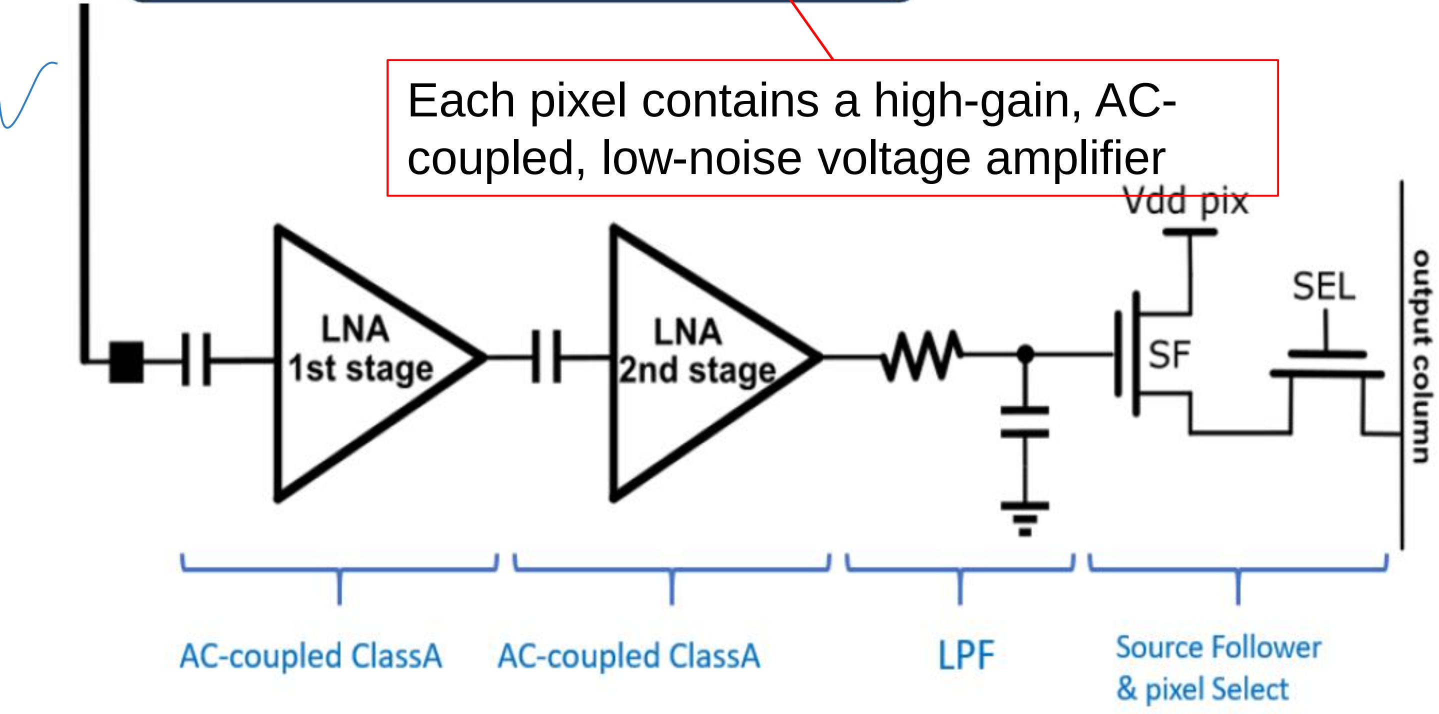


Bundle after Pressing



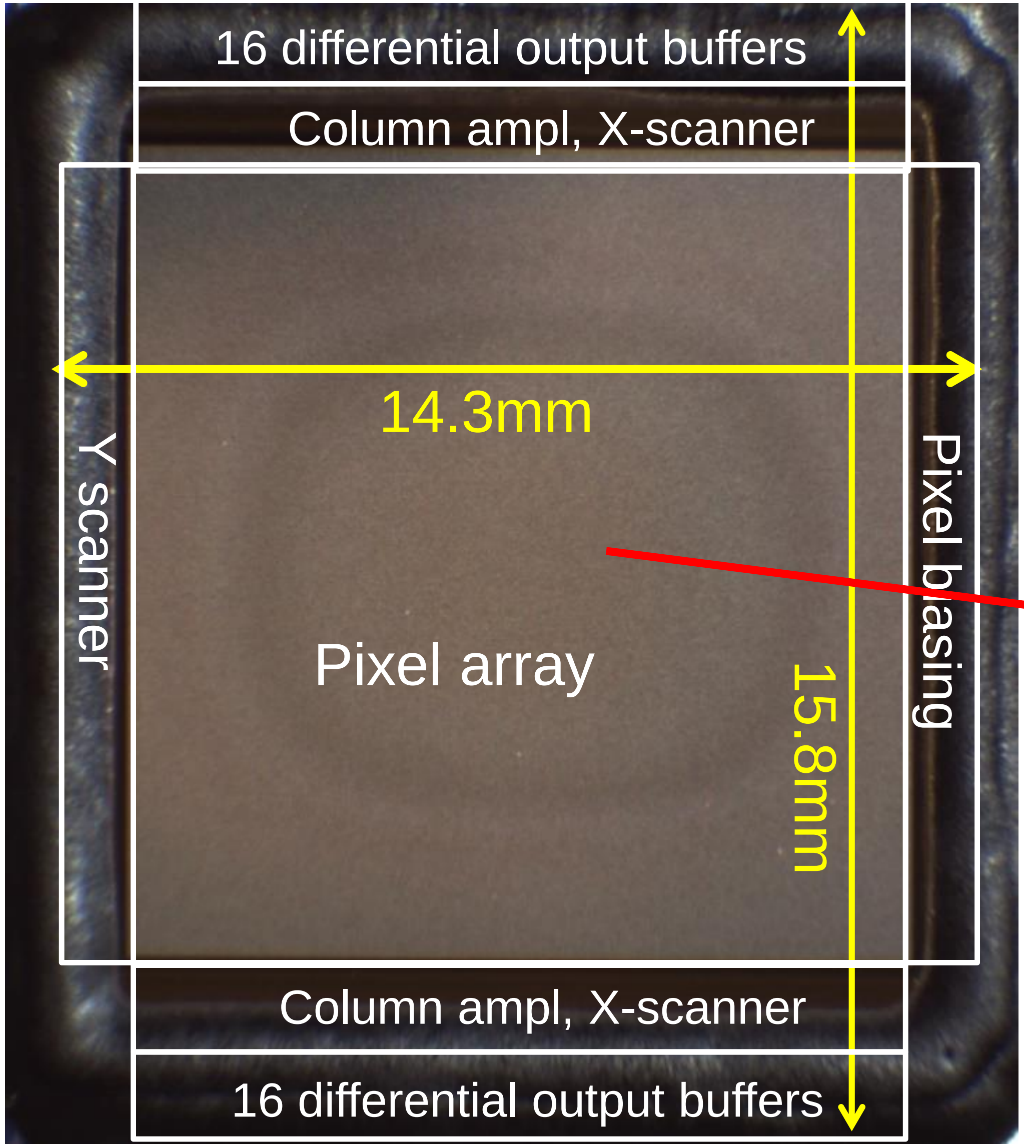
Henry/Argo sensor array



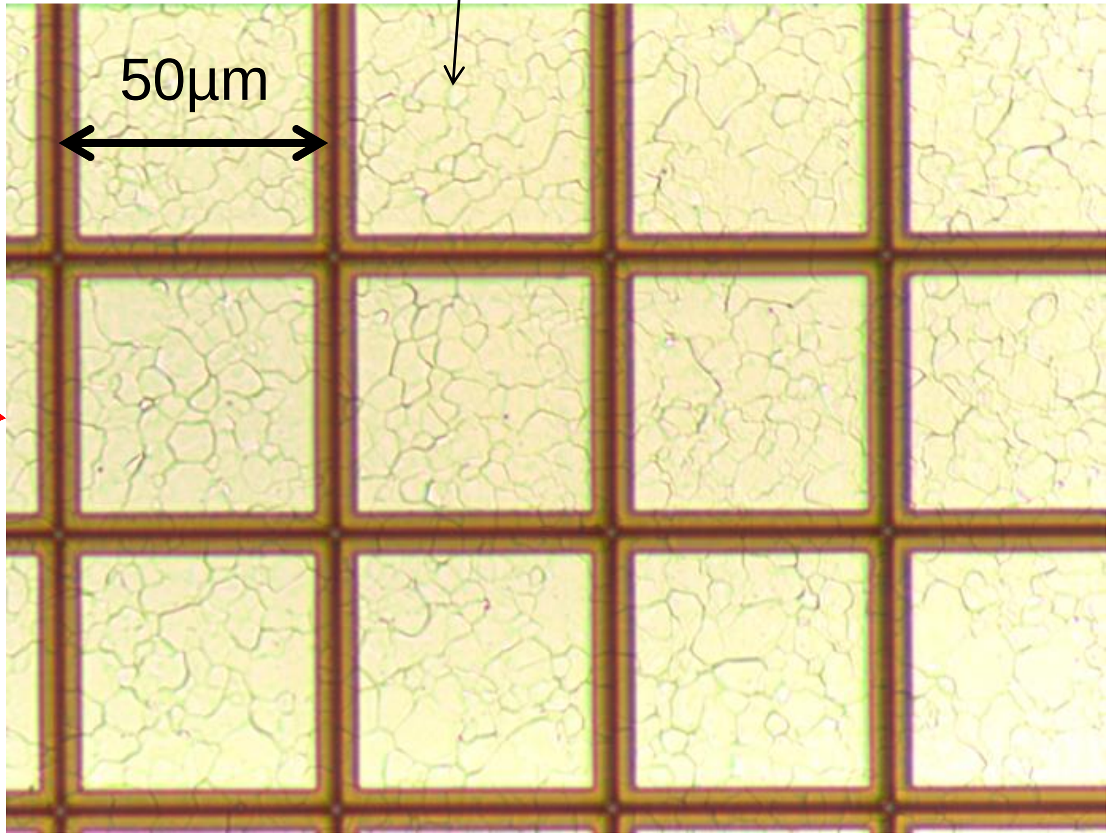


Parameters	Specifications
# of neural sensors	65,536 (256x256)
Full frame readout	up to 39,000 frames/s on 32 analog outputs
Input referred noise	< 10 µVrms (100 Hz- 20 kHz)
Voltage gain	100 – 800 V/V
Input impedance	> 1 TΩ
Pixel pitch	50 mm

Henry



Top electrode to be hybridized to the microwire electrode

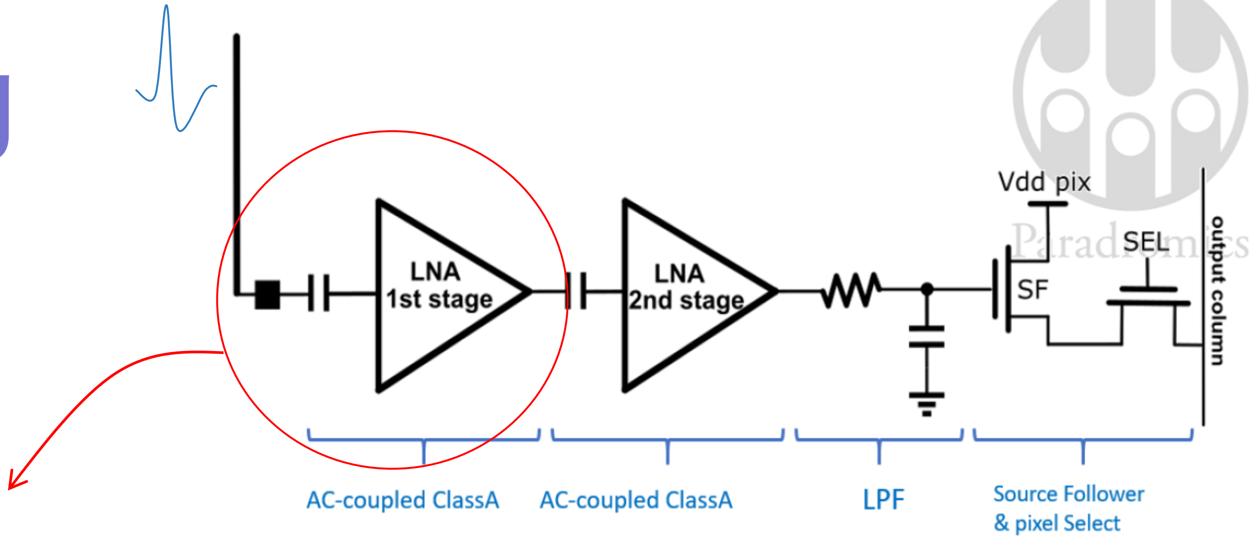


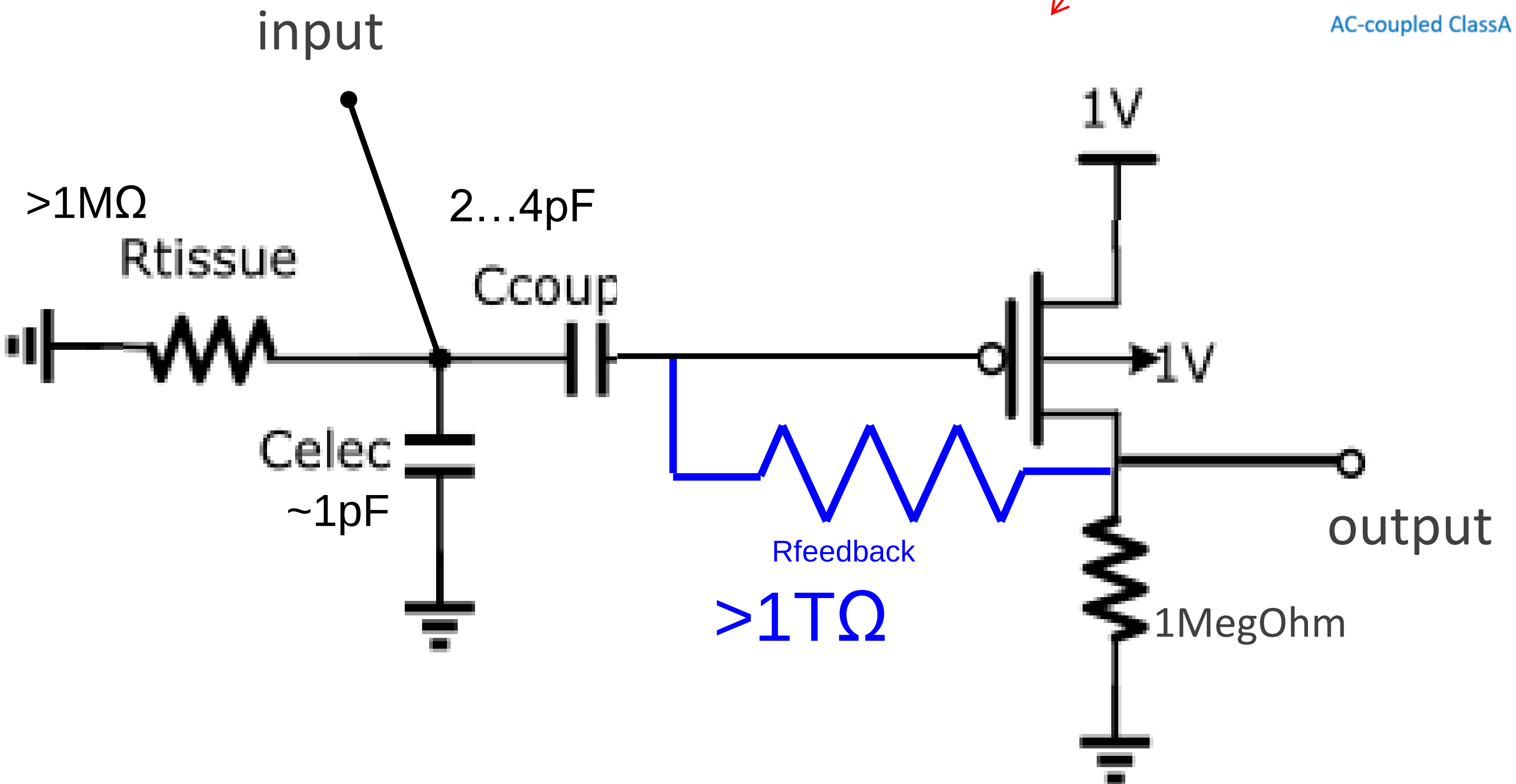
2. Pixel design & performance

→ overall pixel topology
→ design for compactness & for low noise
→ sense amplifier
→ pixel layout
→ measured performance in the array

Class-A amplifier with resistive self-biasing

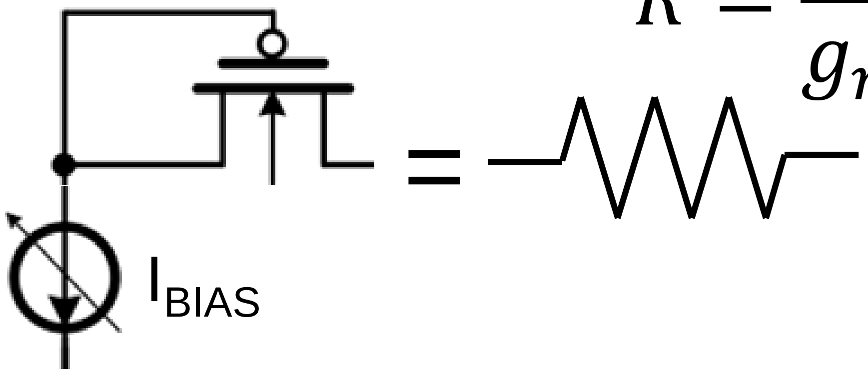
Optimized for 1/f noise: single PMOSFET

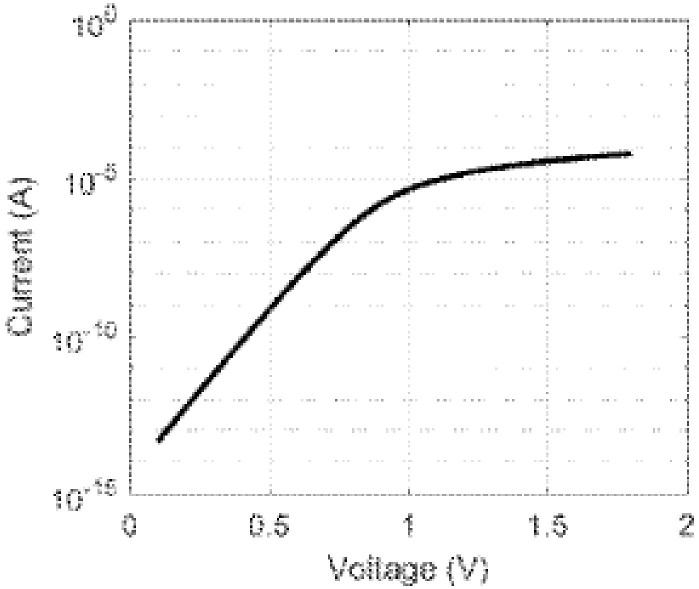


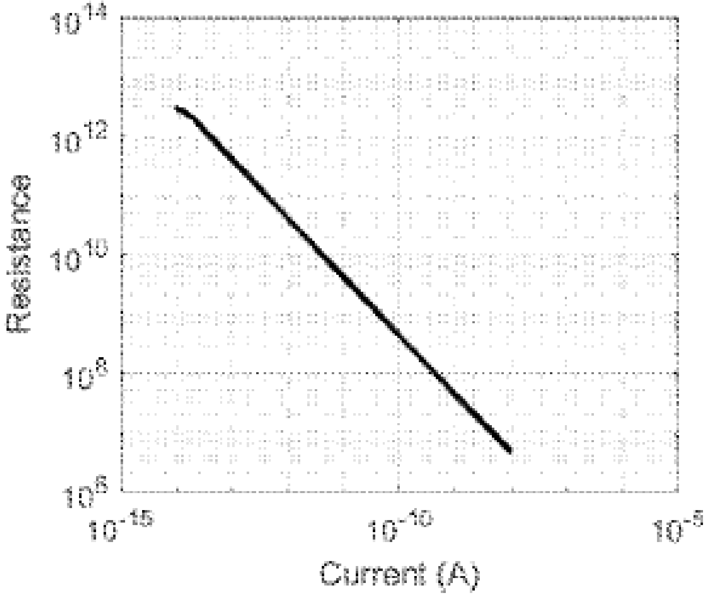


Compact high value resistor

$$R = \frac{1}{g_m} = \frac{kT}{q.I_{BIAS}}$$







PRO

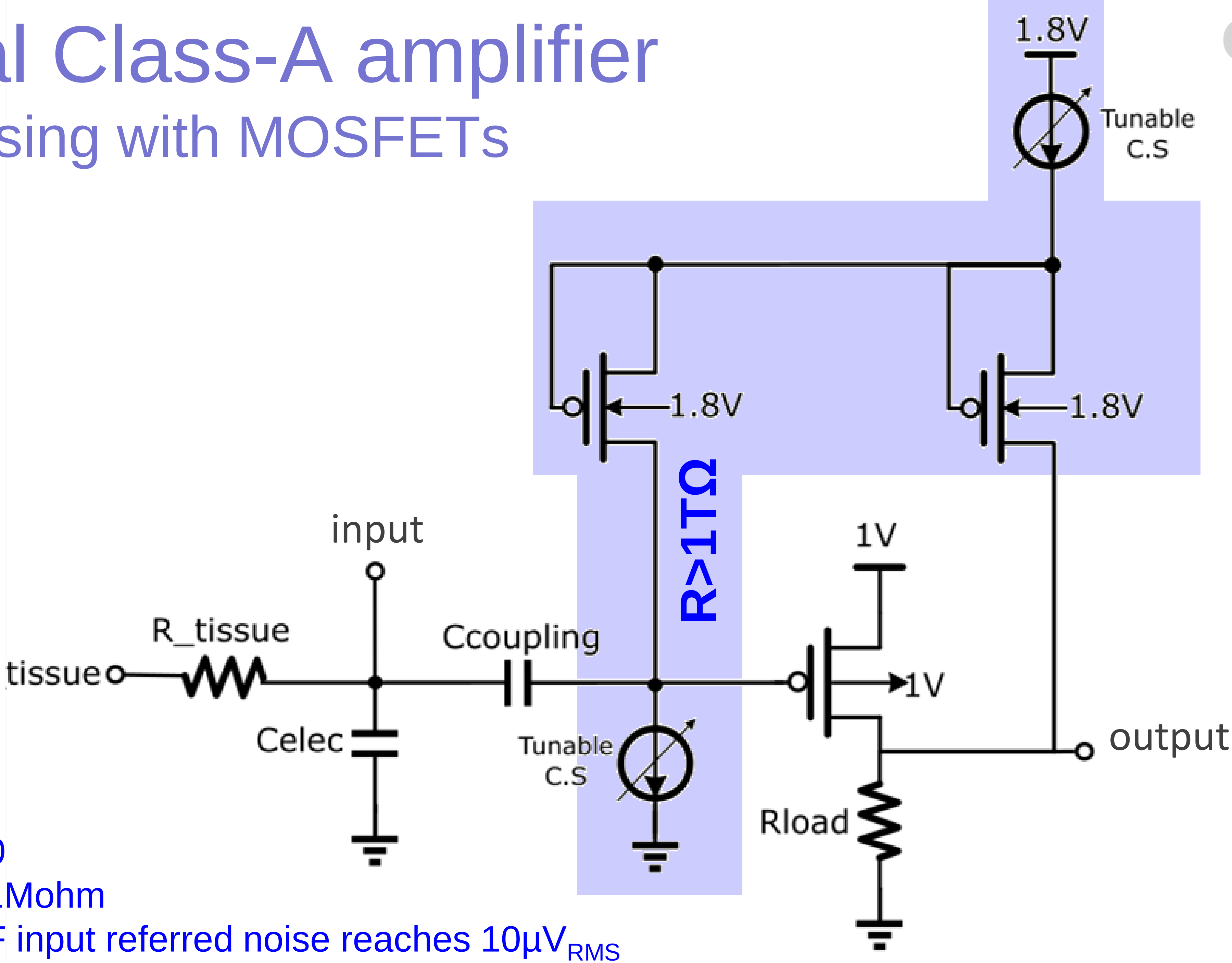
- Compact: a diode-connected MOSFET + a MOSFET bias current source
- $R=1/g_m$ AC value hardly dependent on variability of the 1st MOSFET. Dependent on the variability of the bias
- Can make extremely high R
  e.g. 1TΩ for I_{BIAS}=25fA.
  Needed to make very low RC time:
  1TΩ*100fC=0.1s

CON

- Needs an exclusive DC path for the I_{BIAS}
- Only AC / small signal: << 100mV
- Not very linear
- Offset must be solved by AC coupling
- 1/f noise

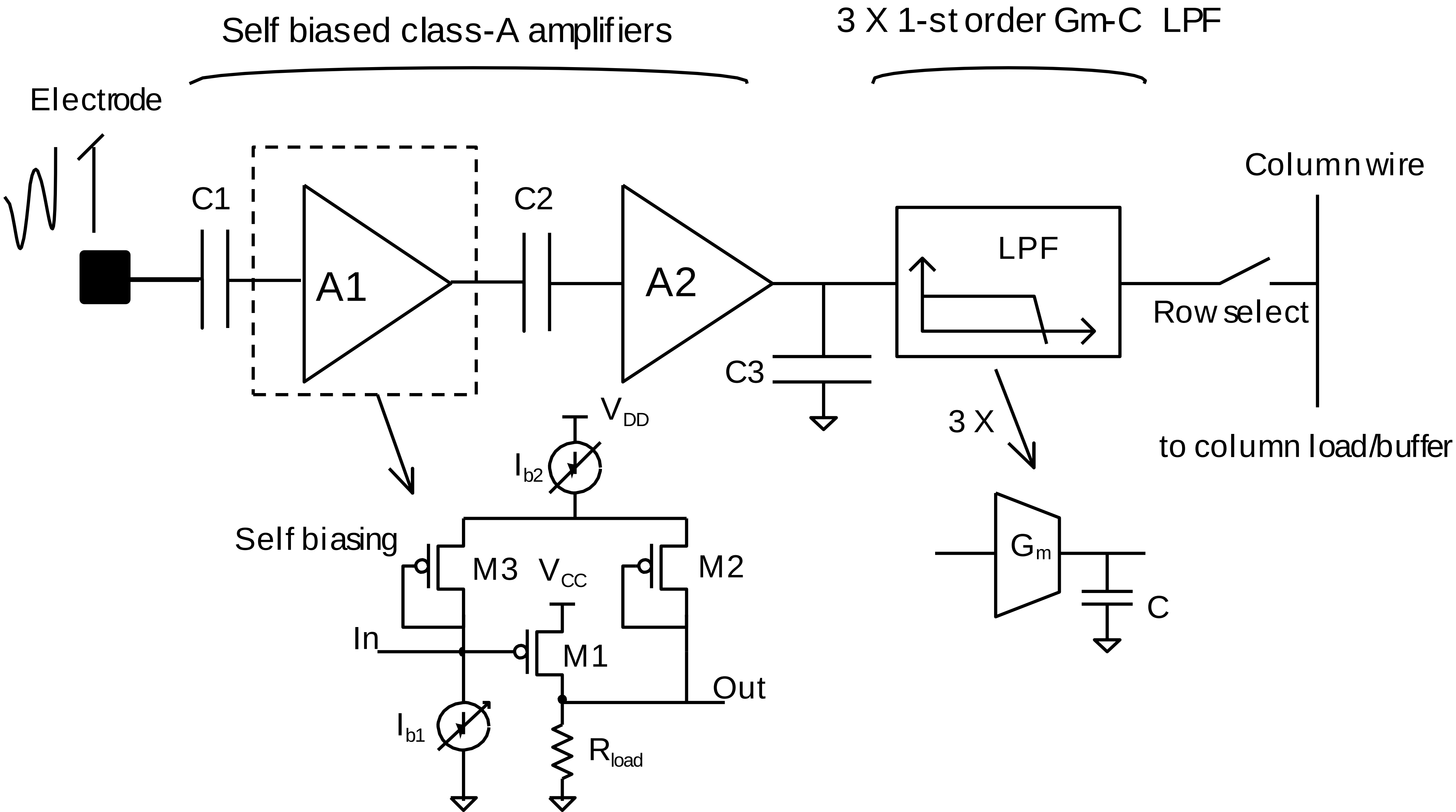
Actual Class-A amplifier

self-biasing with MOSFETs

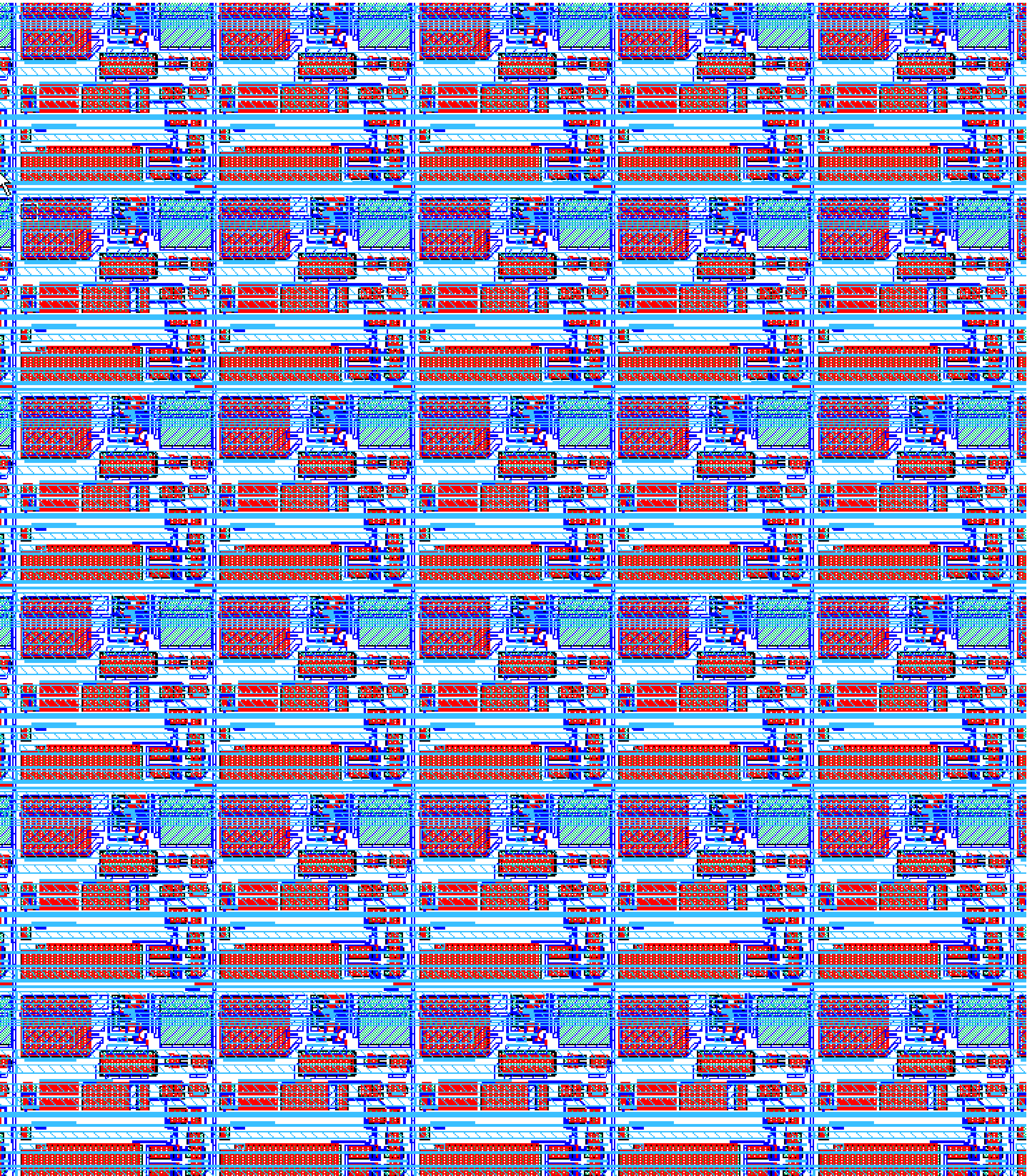


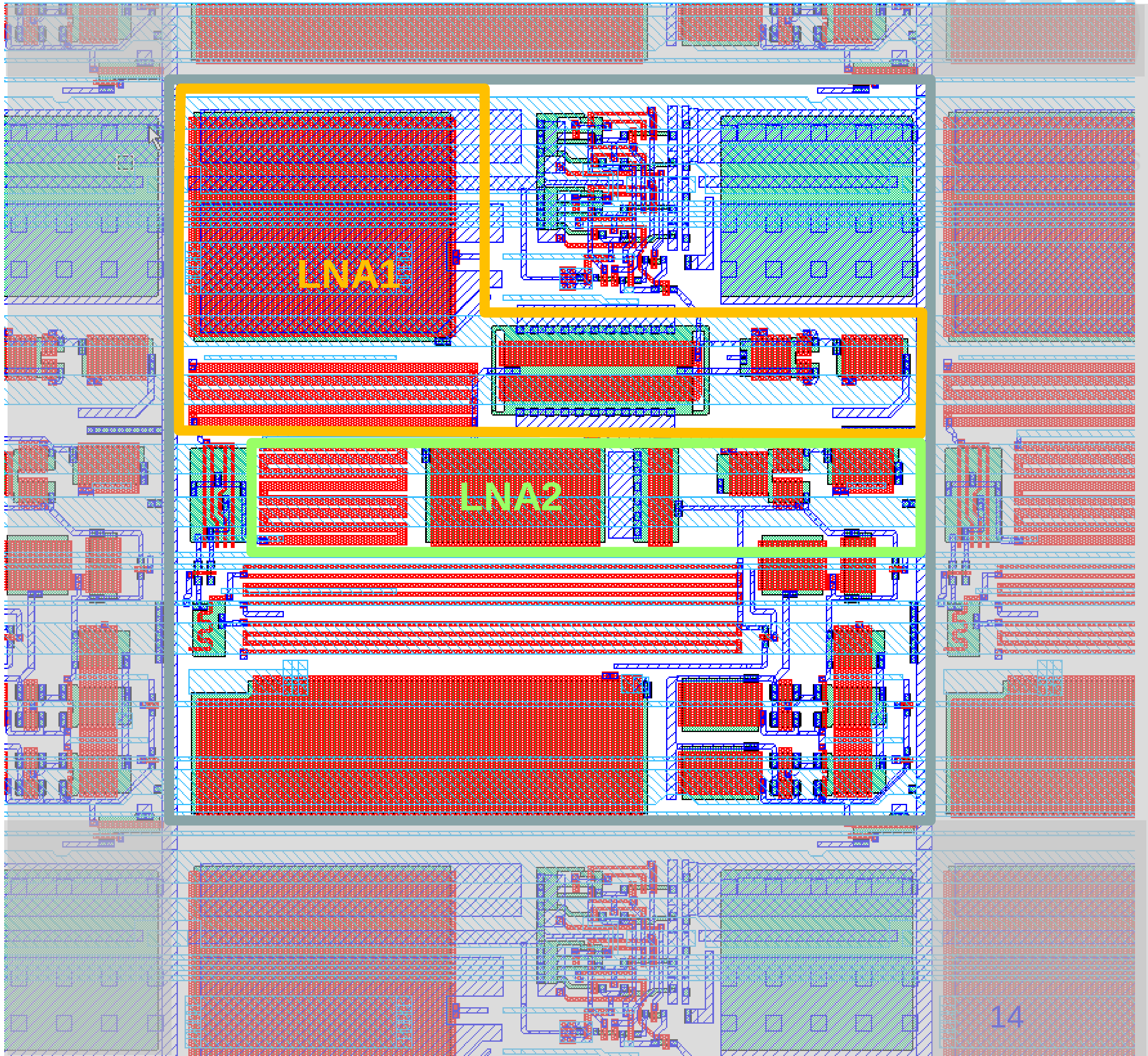
- Gain = 10
- Rload = 1Mohm
- LNA+LPF input referred noise reaches 10µV_{RMS}

Actual Henry pixel topology

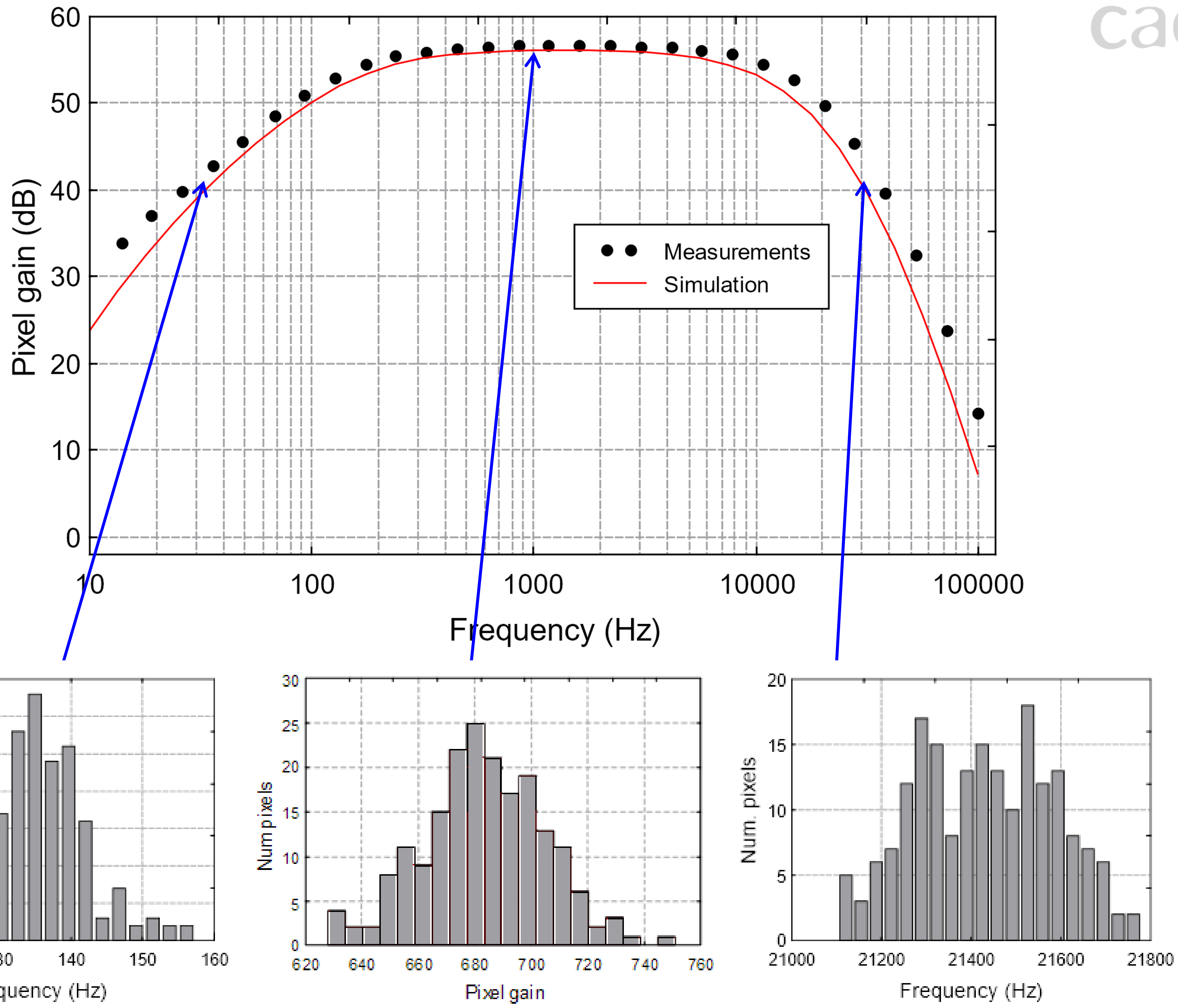


Henry pixel





Total pixel gain and BW



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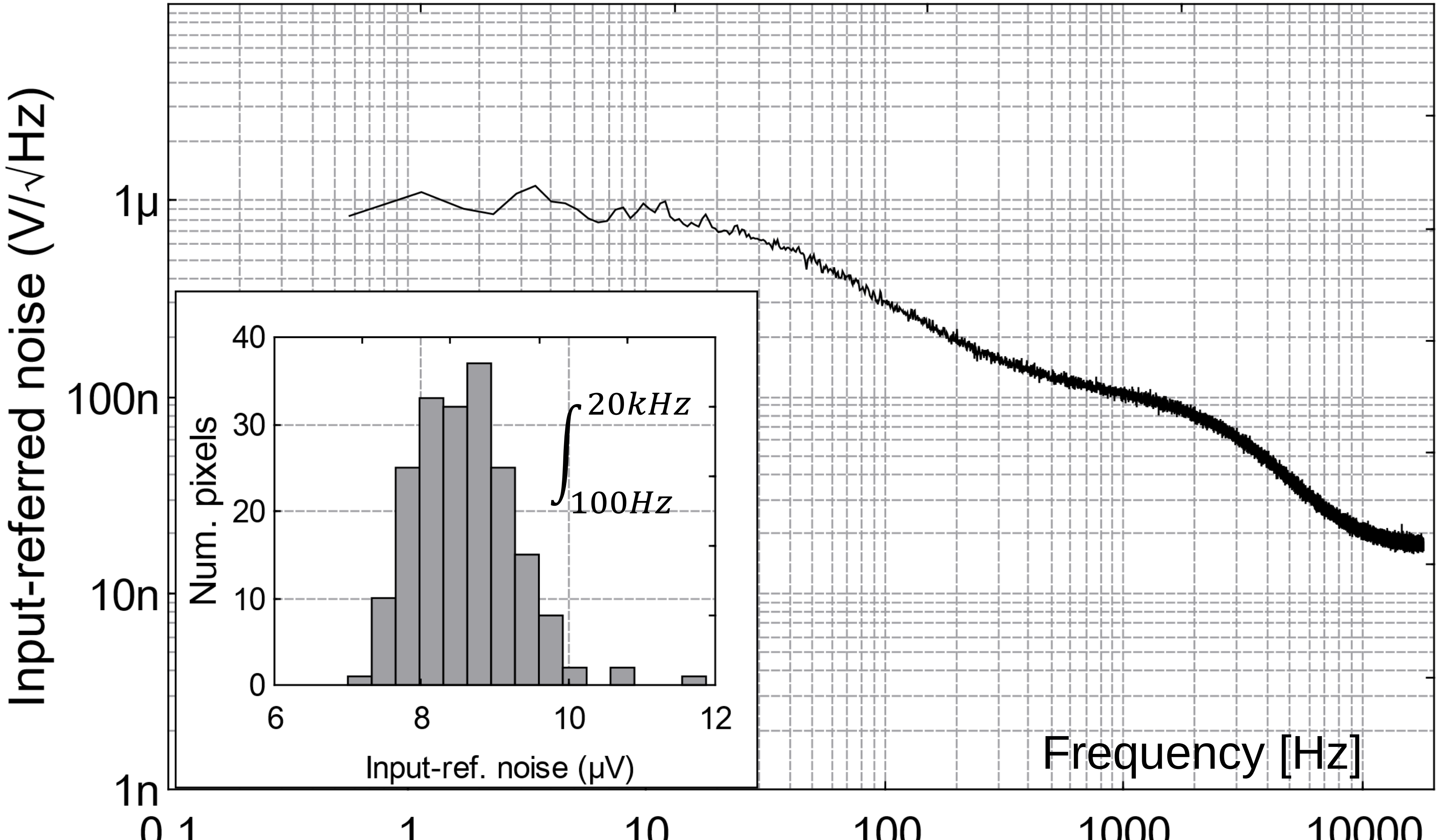
PSD + input noise histogram



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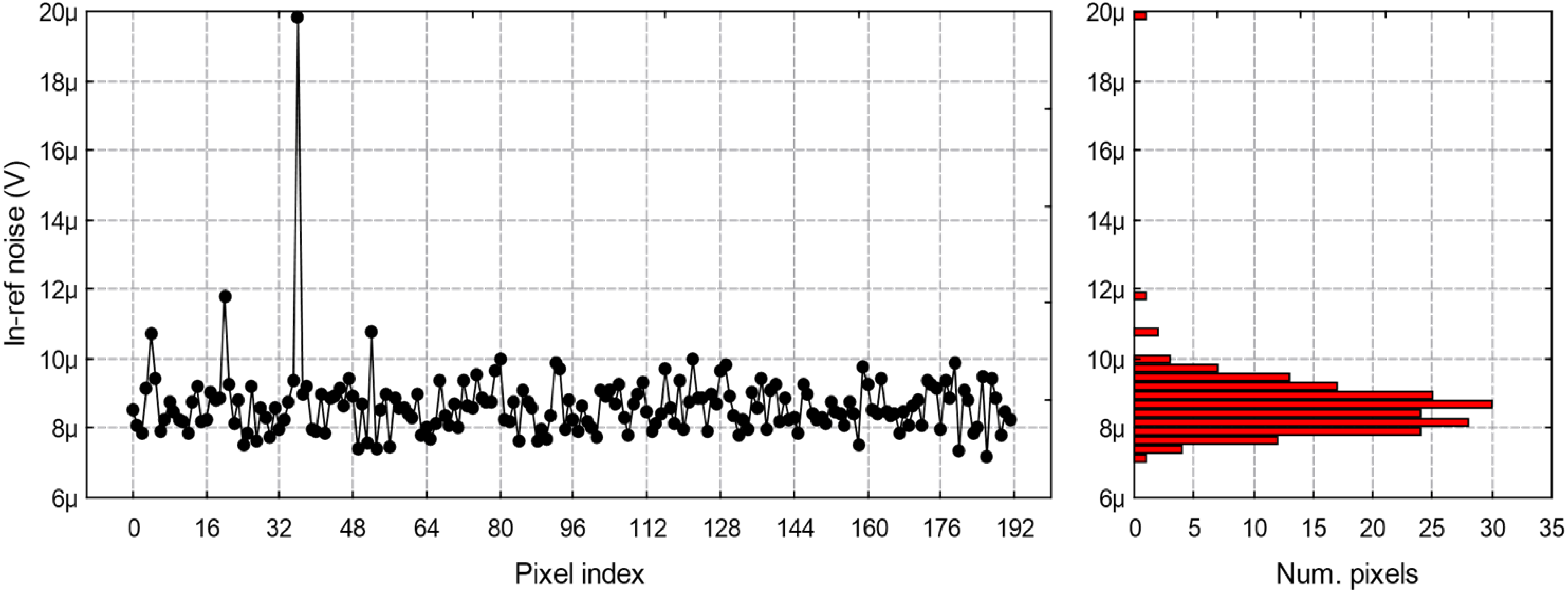
Henry pixel noise
input referred noise of one row of pixels



3. Future outlook

→ recognize pulse shapes by matched filters
→ design of programmable filters
→ measured performance of prototypes

Data reduction == recognize these shapes

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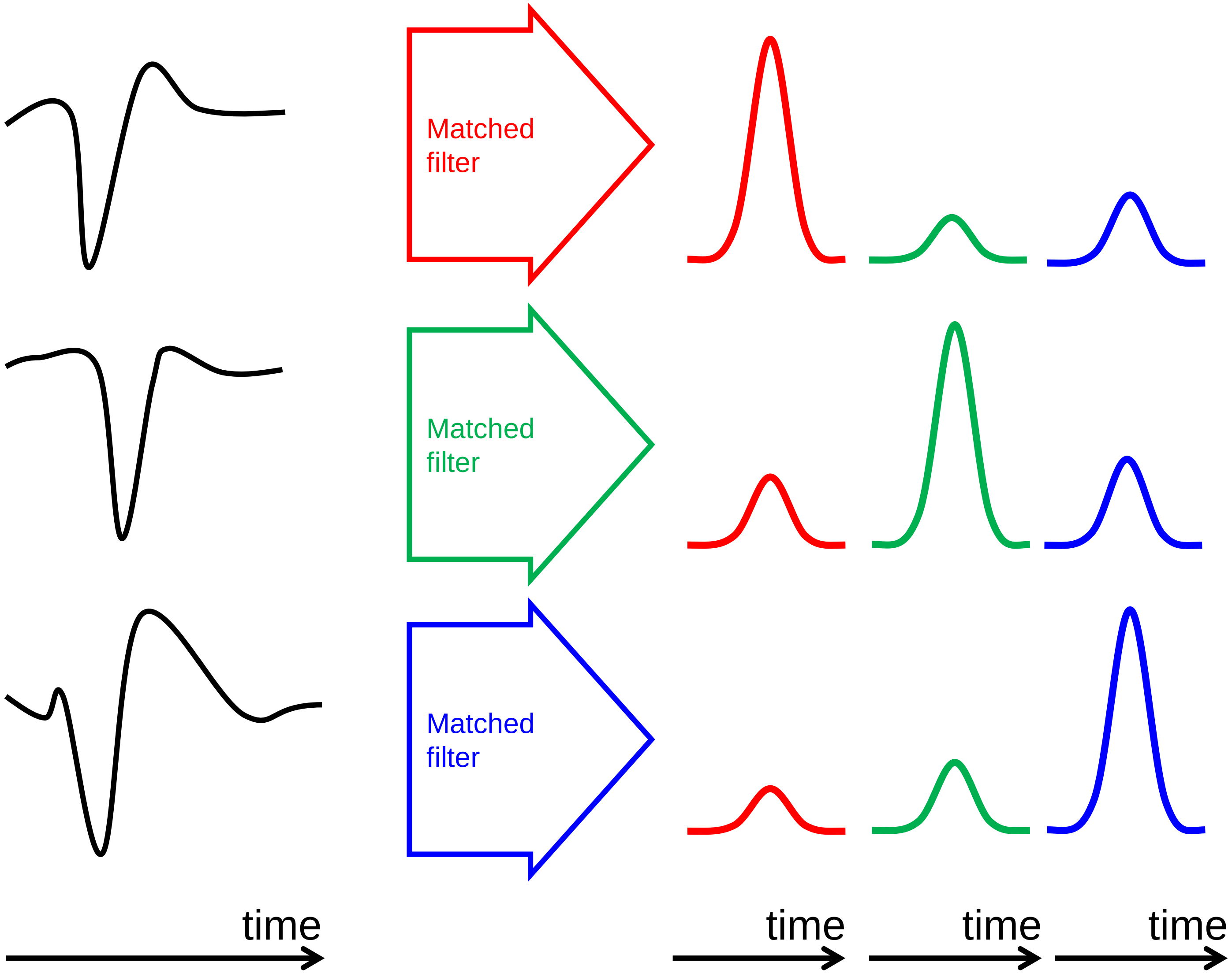
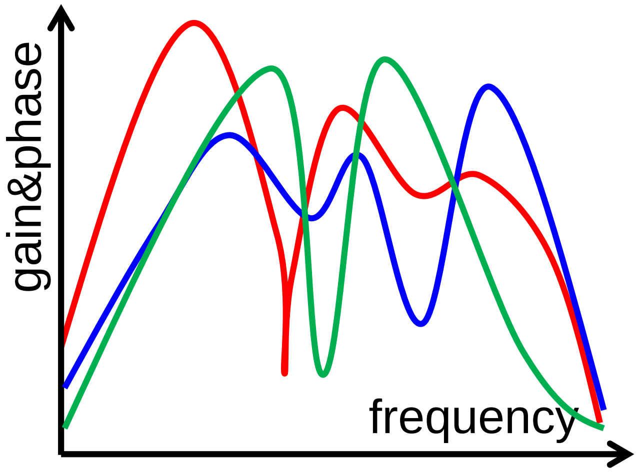
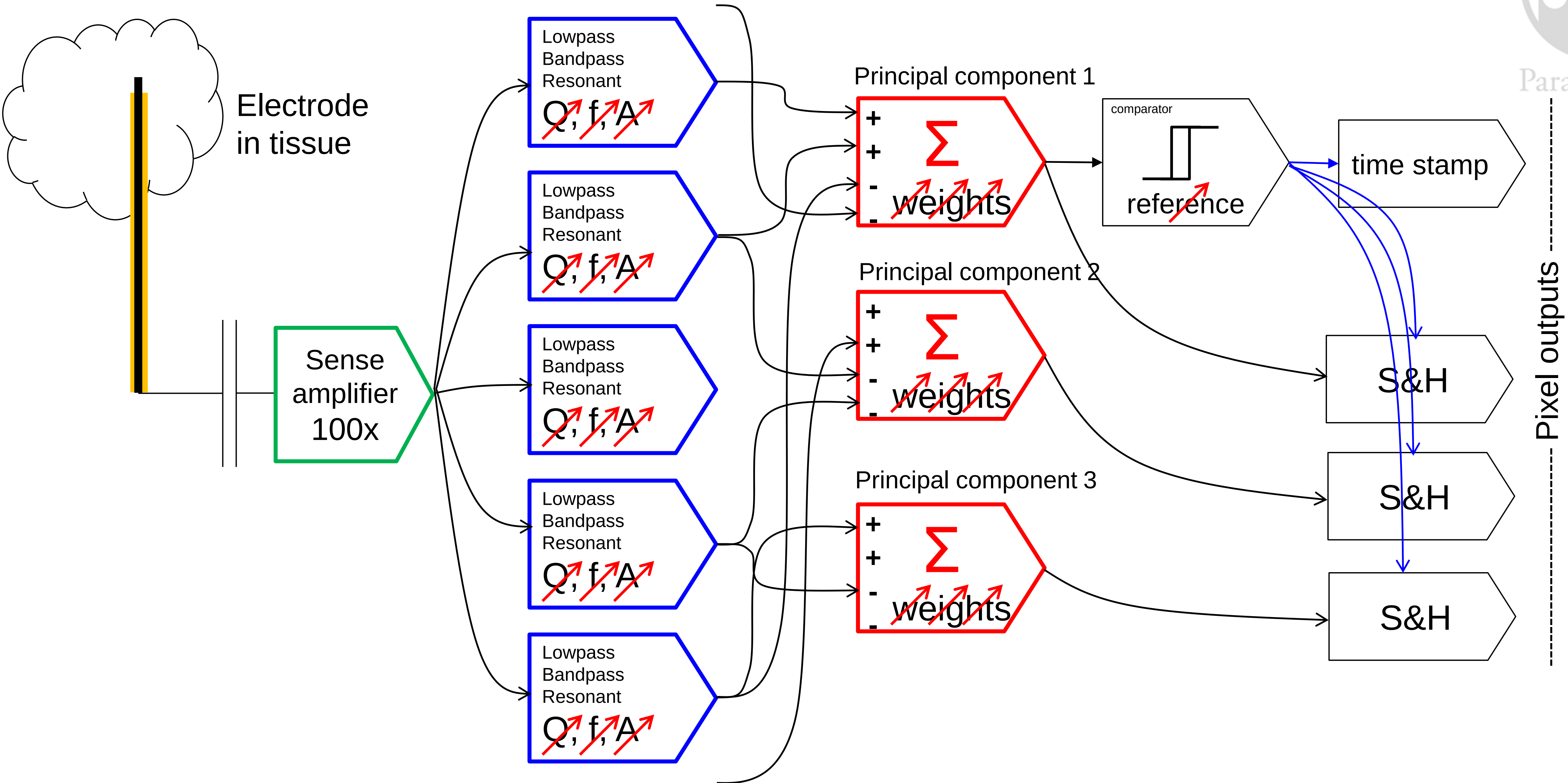




“matched filters”

Approximated by a linear sum of 2nd order filters

Pixel topology



Programmable filters

Filters

- (resonant) bandpass filter
- (resonant) lowpass filter
- summator

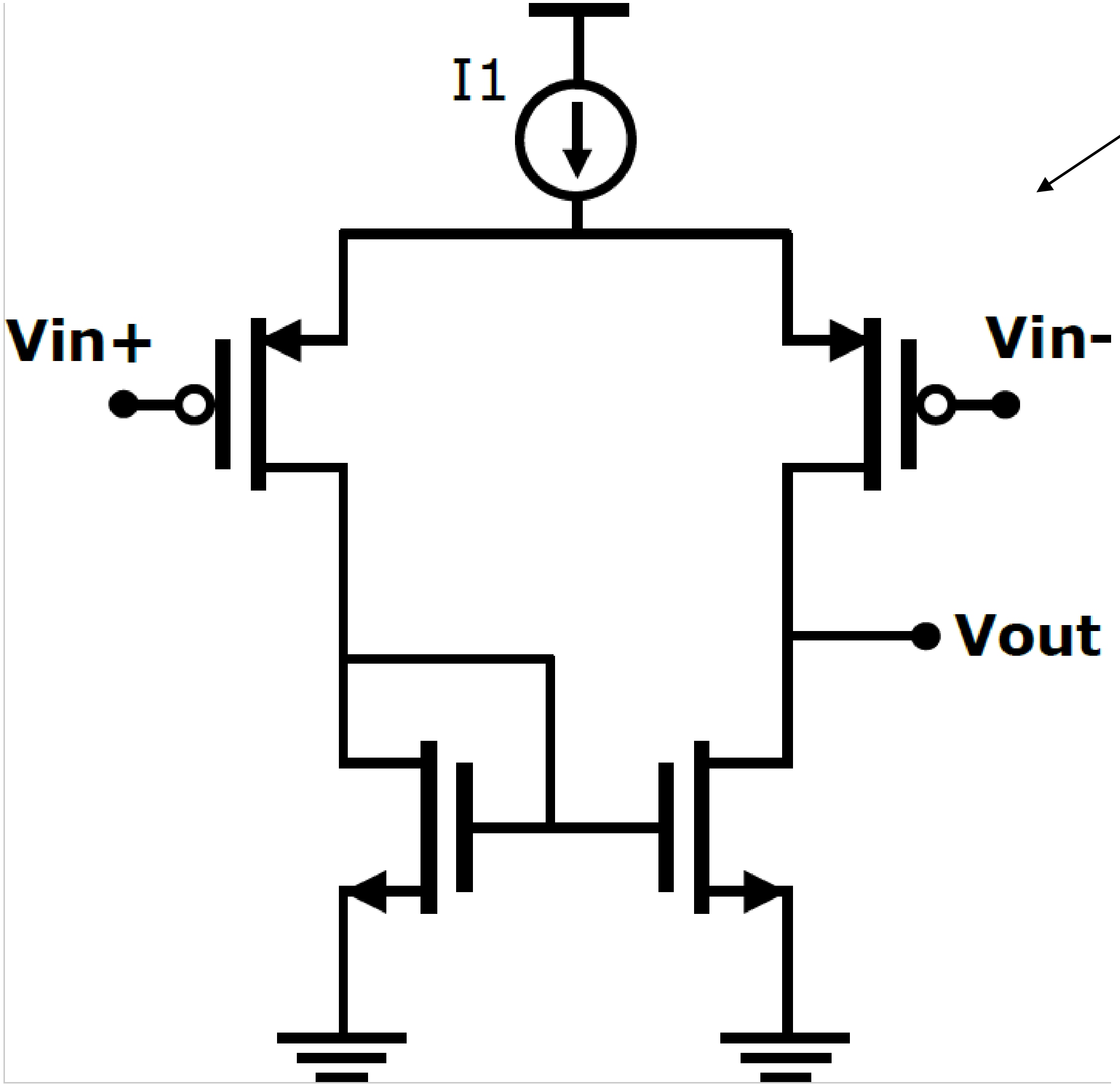
Based on “ideal” R+C active filters

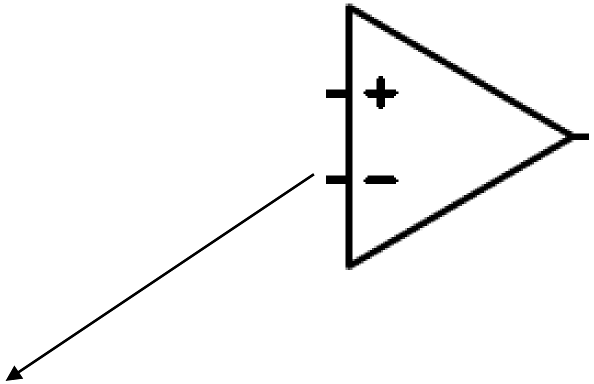
Actually I_{BIAS}/g_m+ C implementations

Continuous programmability of center/lowpass frequency, Q and gain, by programming I_{BIAS}

Patent WO 2018/191725 pending

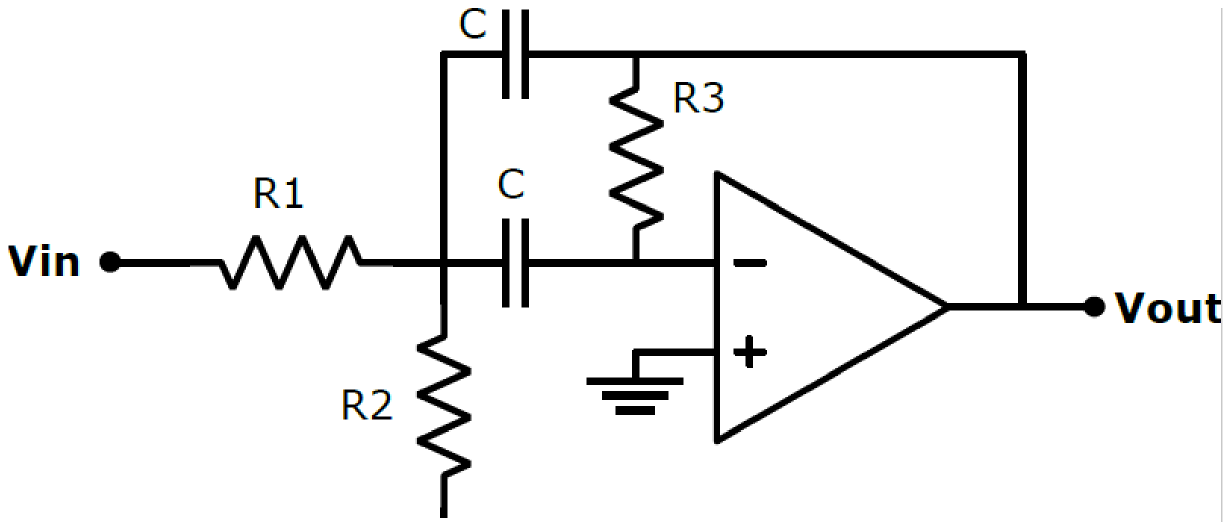
The OTA

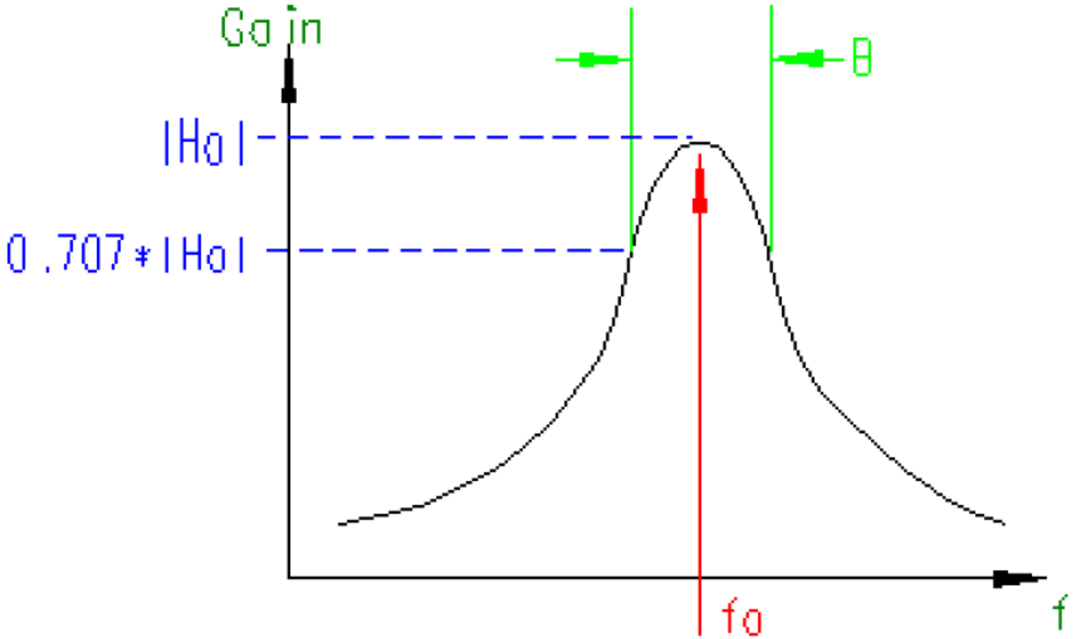




- All transistors are minimum sized, or larger for mismatch
- Tail current can be adjusted between <1fA and >1µA
- Gain = between 100x and 200x

Resonant bandpass filter (ideal)





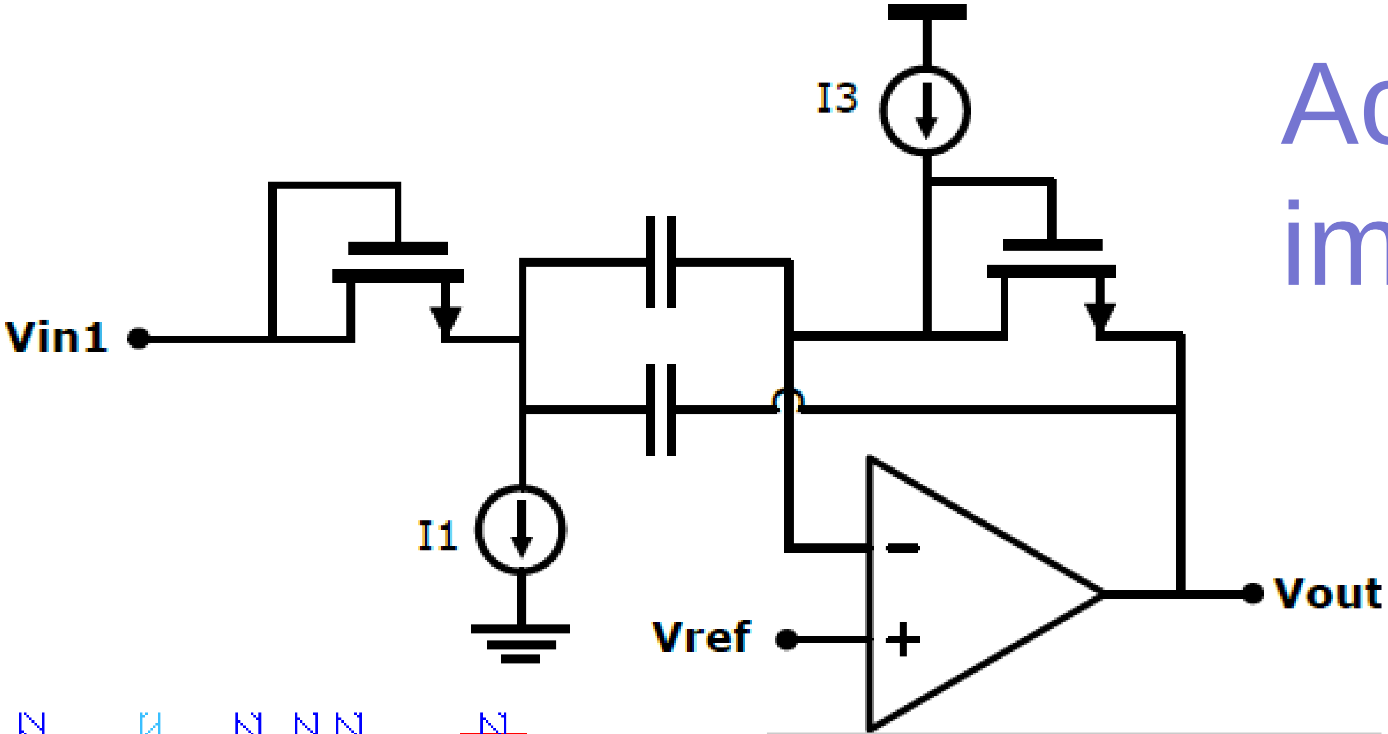
Bandwidth = β

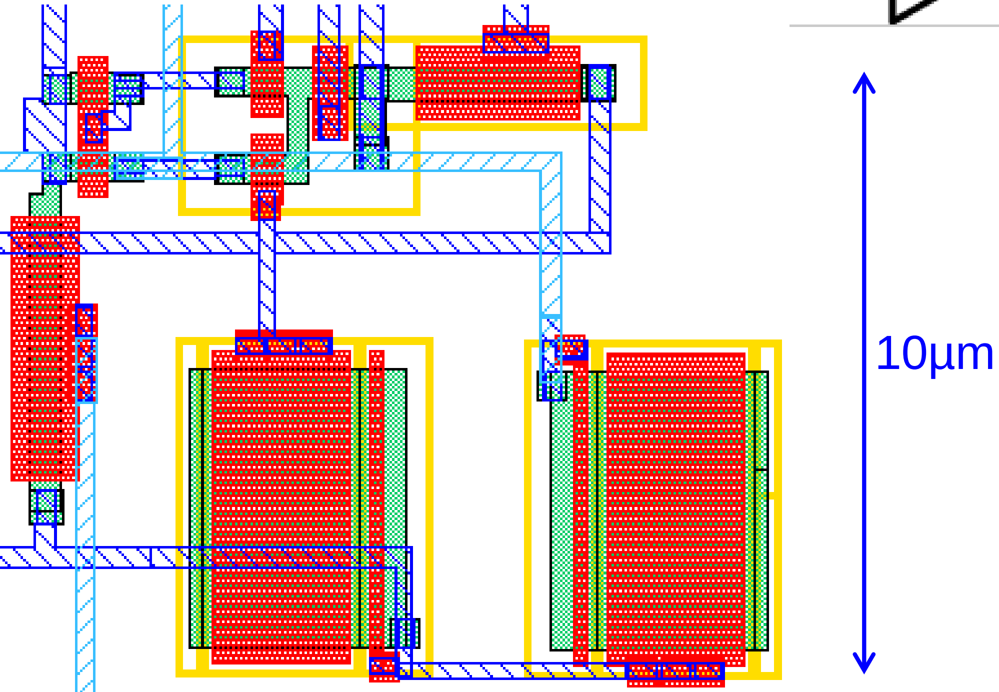
Quality factor = ω_0/β

$$H_o = -\frac{R_3}{2R_1}$$

Radian frequency	Hertz
$\omega_o = \frac{1}{C\sqrt{(R_1 \| R_2) R_3}}$	$f_o = \frac{\omega_o}{2\pi}$
$\beta = \frac{2}{CR_3}$	$B = \frac{\beta}{2\pi}$

Actual implementation



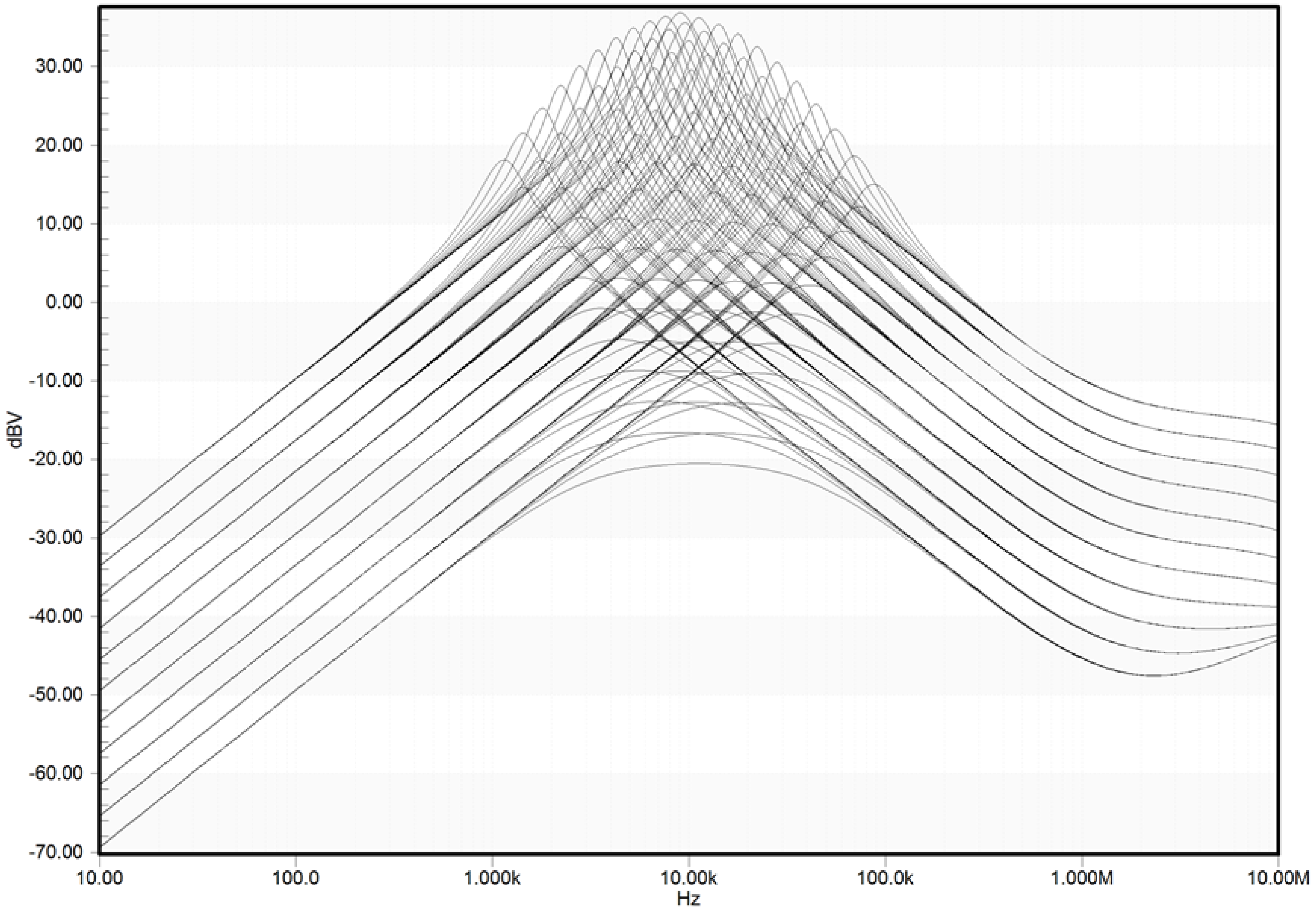


Pro: compact layout
Pro: easy to implement, pure MOS
Pro: input offset free
Pro: programmable by current
Con: one less degree of freedom (R2 absent):

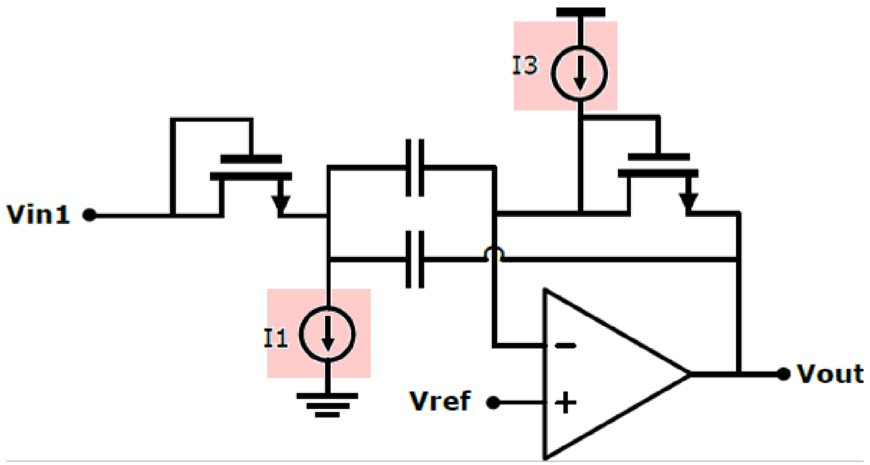
If Q must be large, the difference between the two currents becomes huge.

If Q is too small, the center gain H0 becomes small as well.

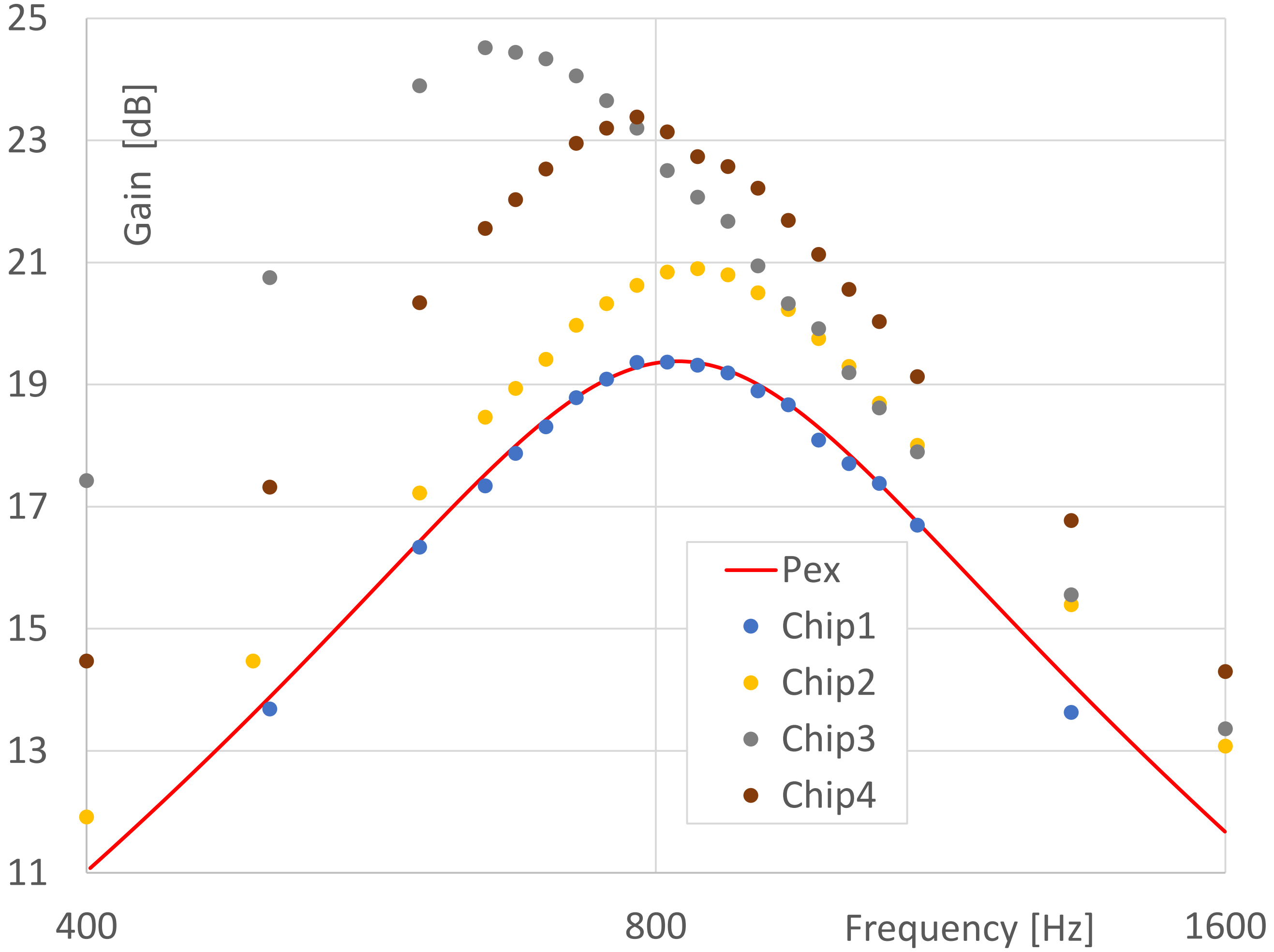
Sweeping both branch currents (simulation)

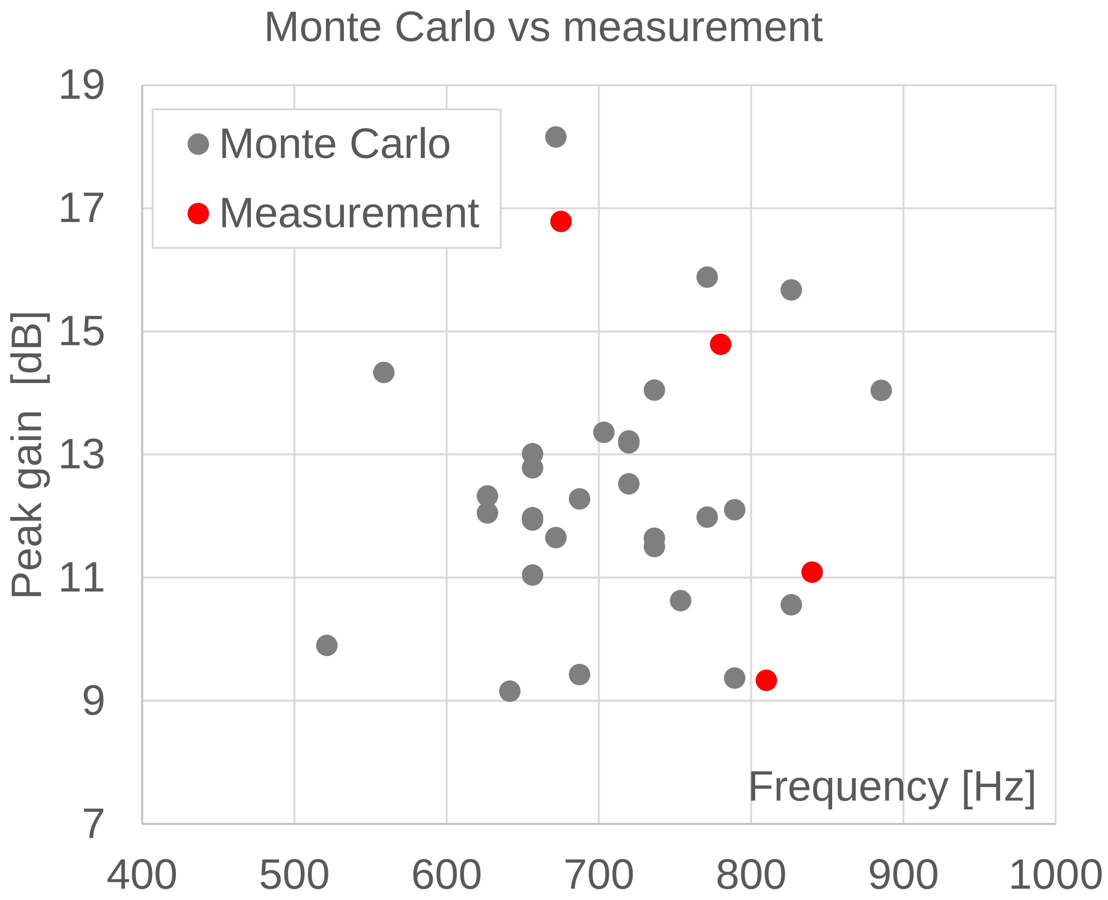


- The two branch currents are adjusted to obtain the desired Q and resonant frequency
- C=100fF

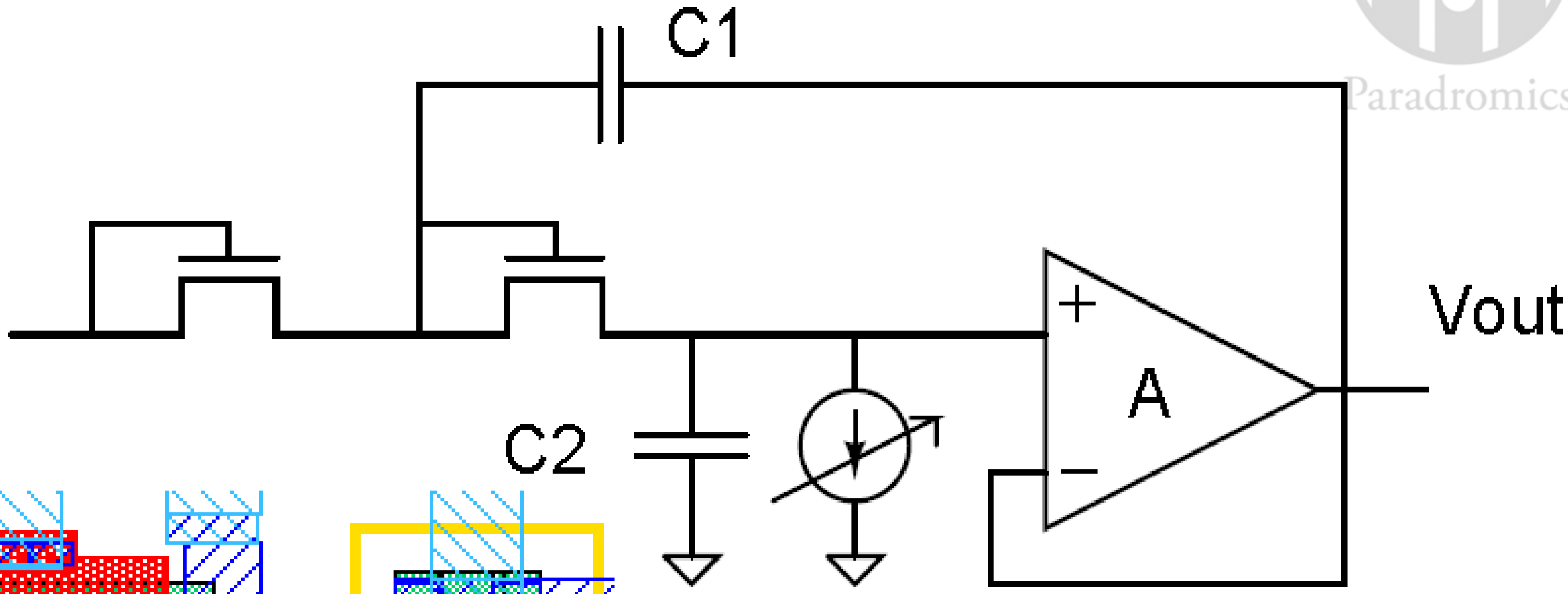


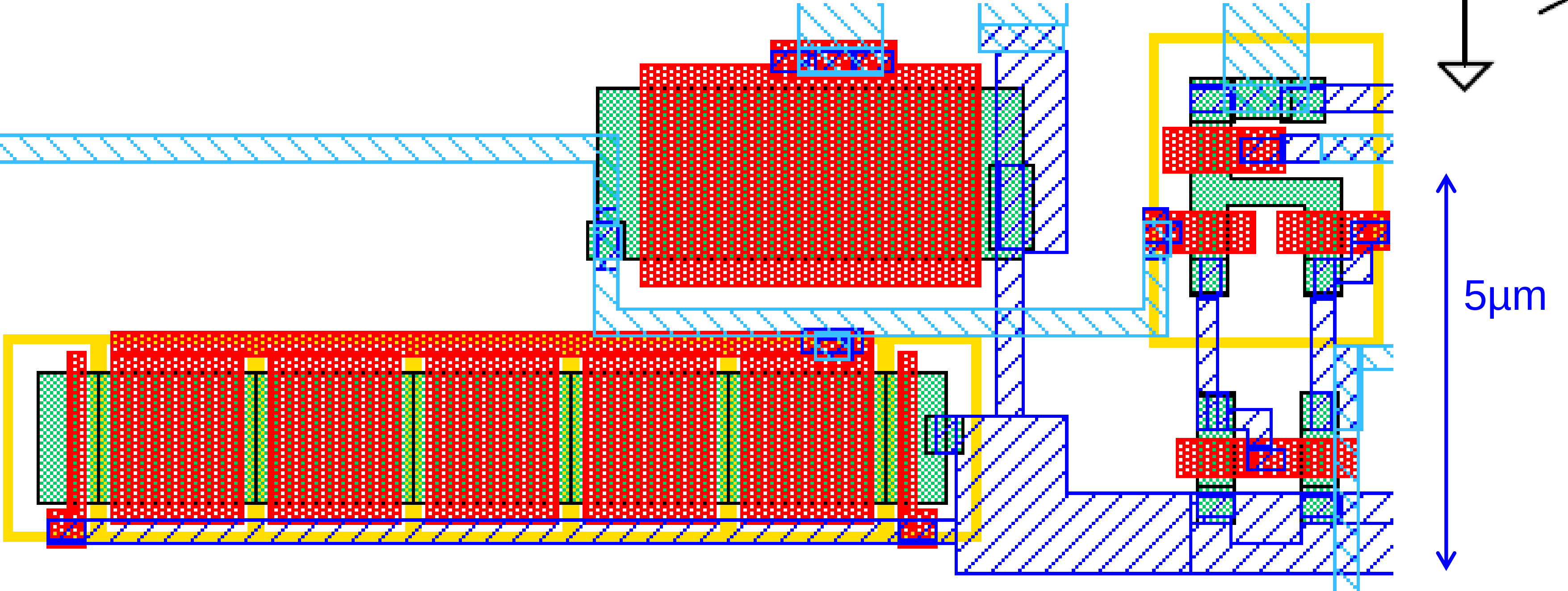
BPF measurement vs simulation



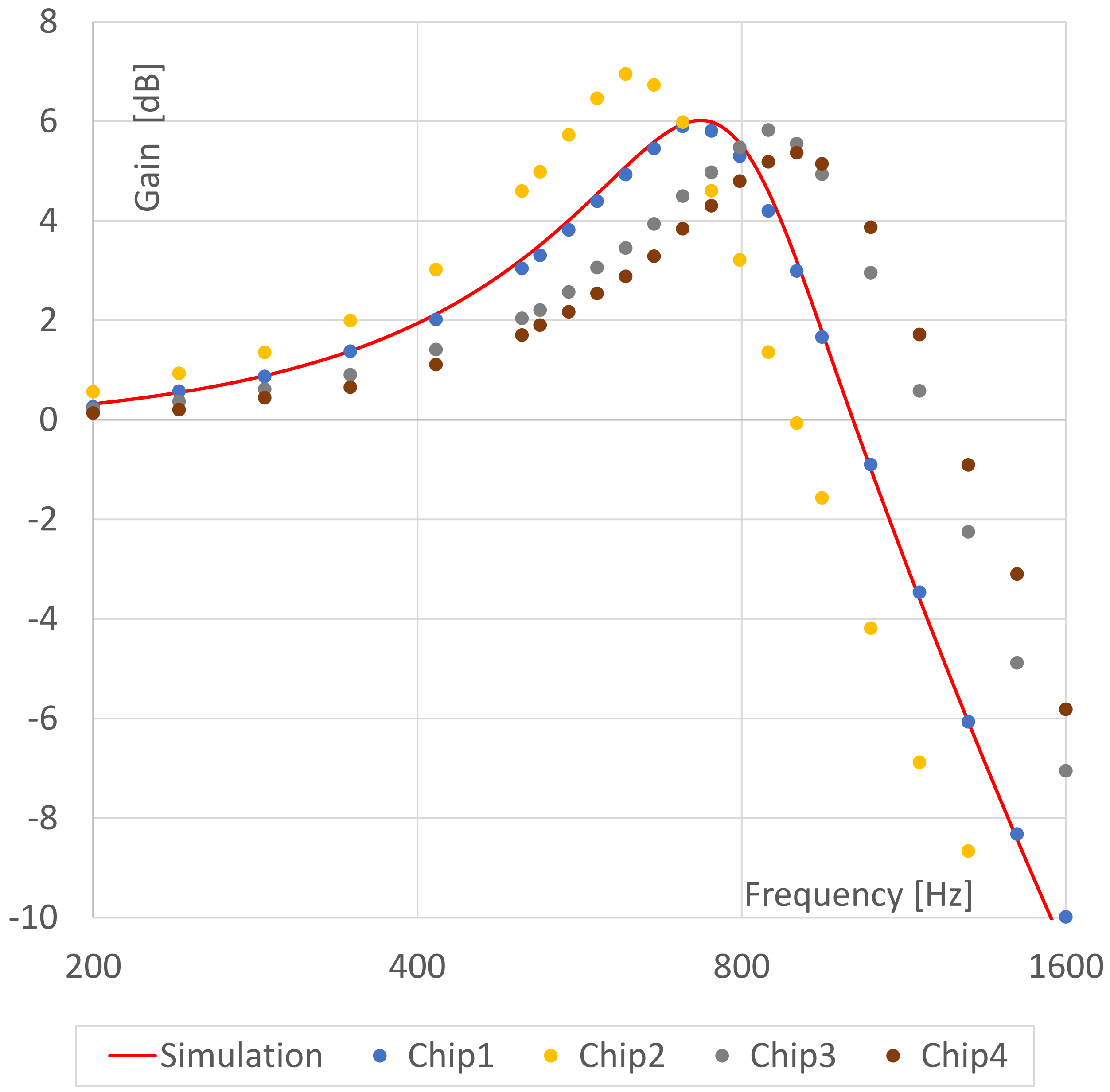


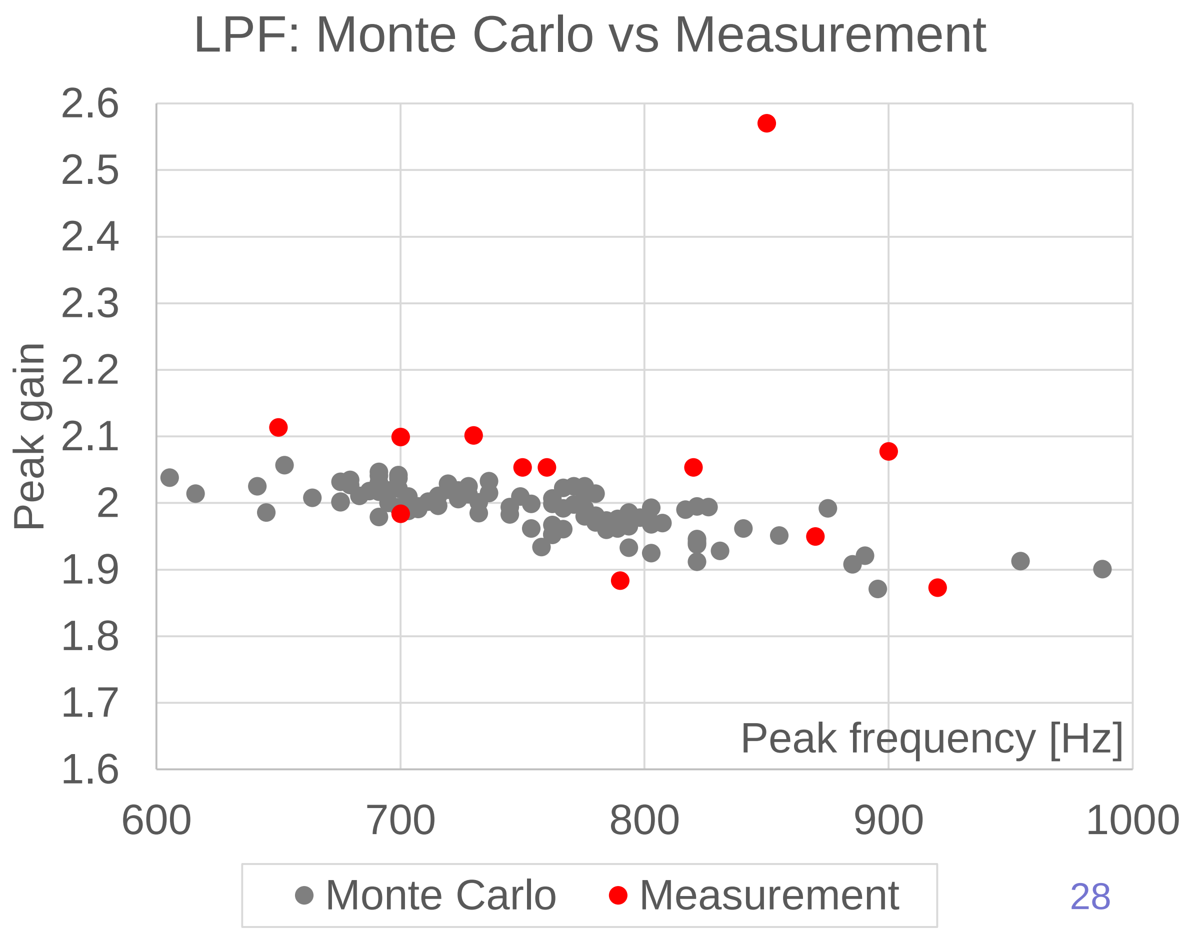
2nd order low-pass filter



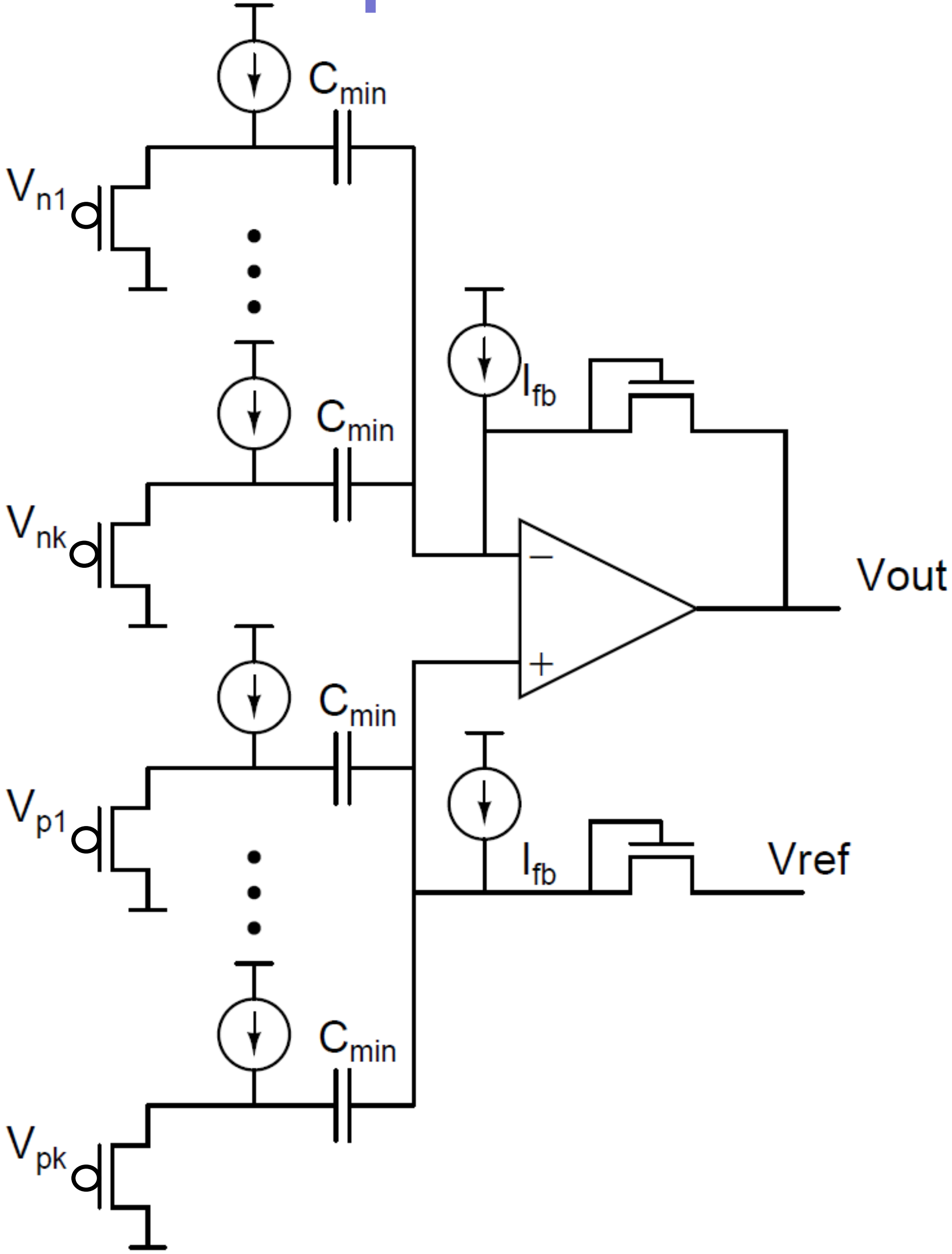


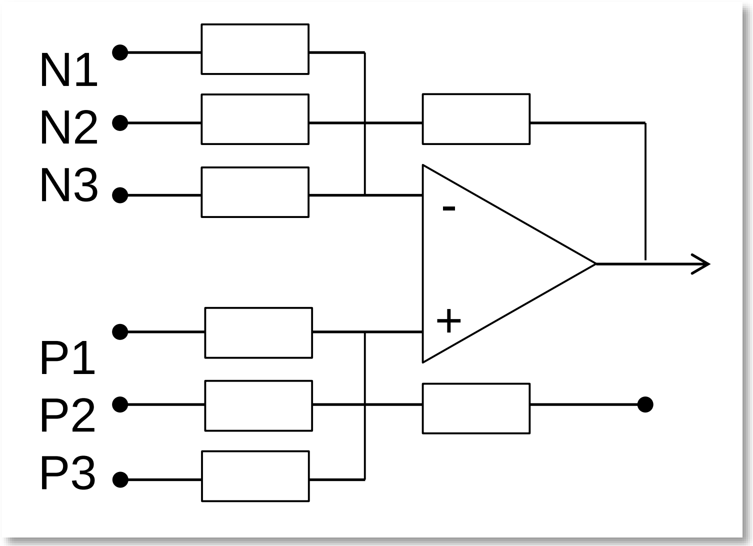
LPF measurement vs simulation





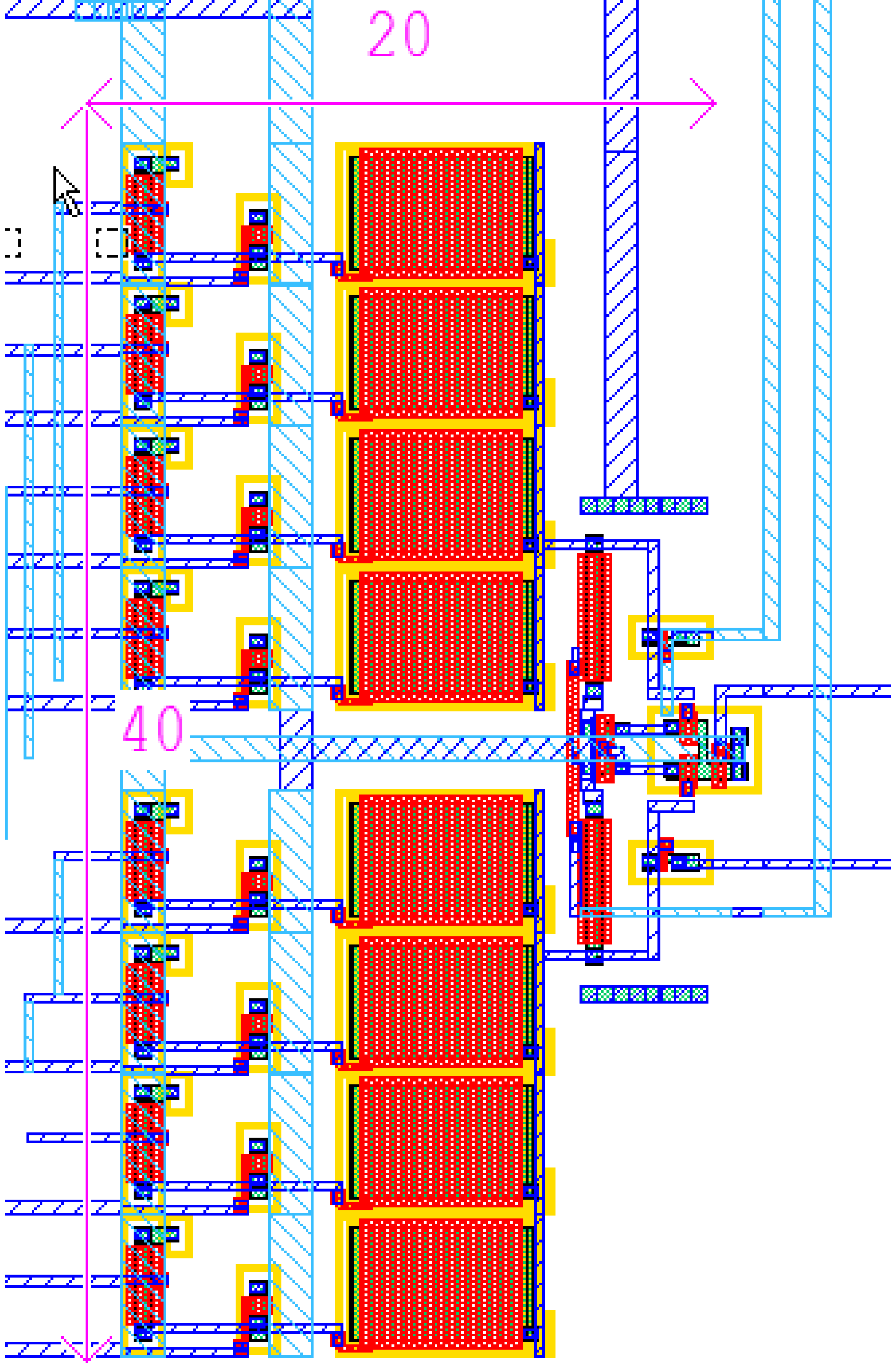
Multi-input differential summator





- Pure MOSFET design
  - All transistors have minimum size (except when needed for matching)
  - Capacitors are 100fF MOS
  - Input stages are PMOSFET source followers
- By adjusting the currents one can set the SF's output impedance, hence the gain of each branch

Summator layout
4 + inputs
4 - inputs



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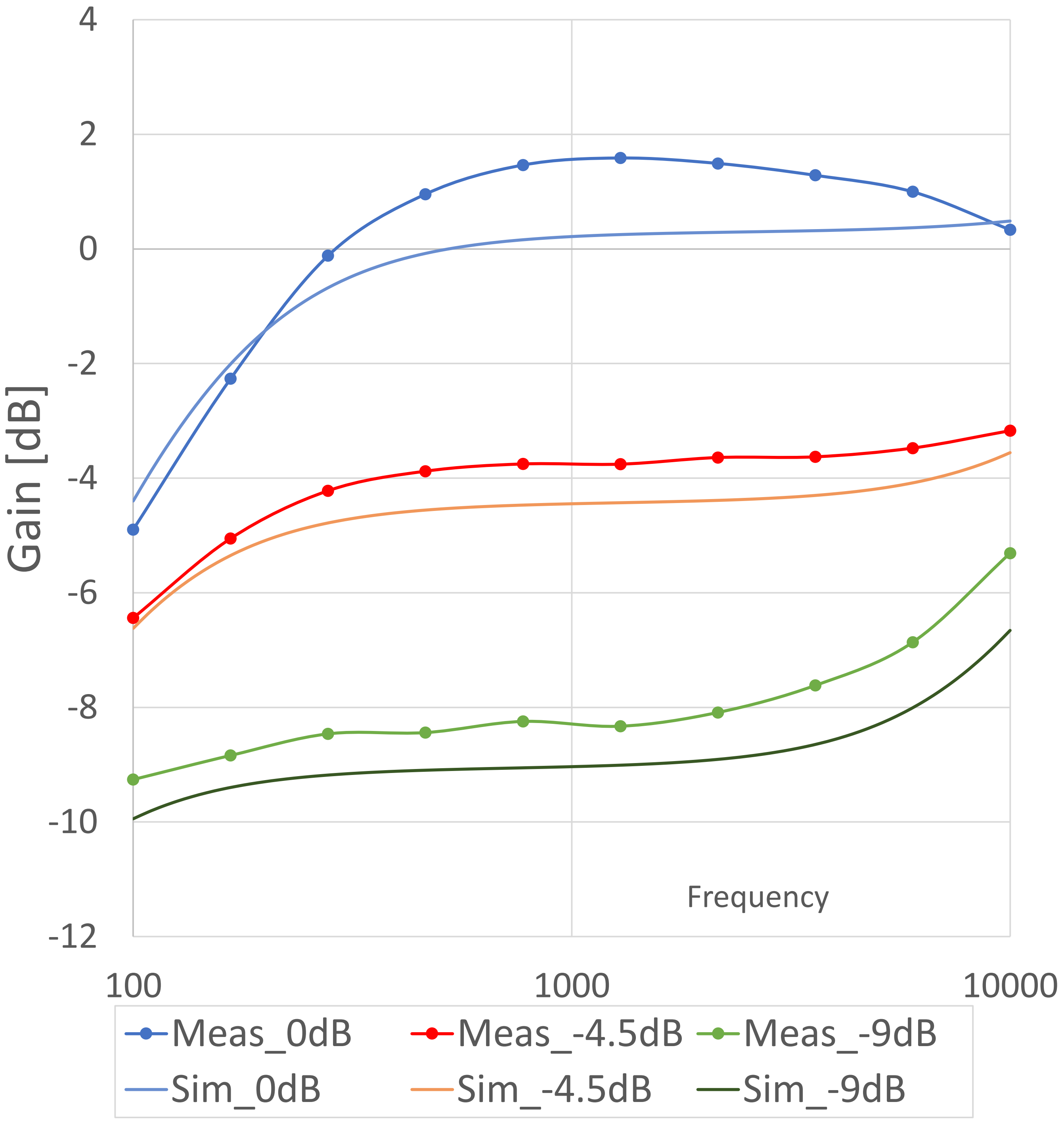

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Summator: simulation vs. measurement

Three different branches with different gains 0dB, -4.5dB, -9dB

Measurement compared with simulation

4 Conclusions

Conclusions

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- Unprecedented massive parallel 256x256, 50µm pitch neural probe ROIC
- 10µV_{RMS} @ 20kHz bandwidth

- Compact, in-pixel analog domain filters demonstrated
- Fully programmable
- Key design issue: mismatch of MOSFETs causes variability of frequency, gain and Q

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Thank you!

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NIH

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Grant Number: 1 R43 MH110287-01
Co-PIs: Angle and Melosh